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(54) **CONFIGURABLE PHYSIOLOGICAL MEASUREMENT SYSTEM**

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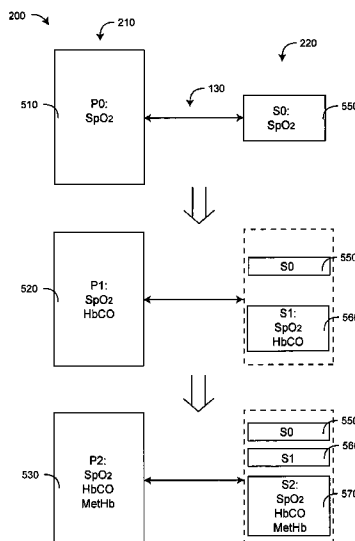
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ABSTRACT

A physiological measurement system has a sensor, a processor, a communications link and information elements. The sensor is configured to transmit light having a plurality of wavelengths into a tissue site and to generate a sensor signal responsive to the transmitted light after tissue attenuation. The processor is configured to operate on the sensor signal so as to derive at least one physiological parameter. The communications link is adapted to provide communications between the sensor and the processor. The information elements are distributed across at least one of the sensor, the processor and the communications link and provide operational information corresponding to at least one of the sensor, the processor and the communications link.

20 Claims, 5 Drawing Sheets



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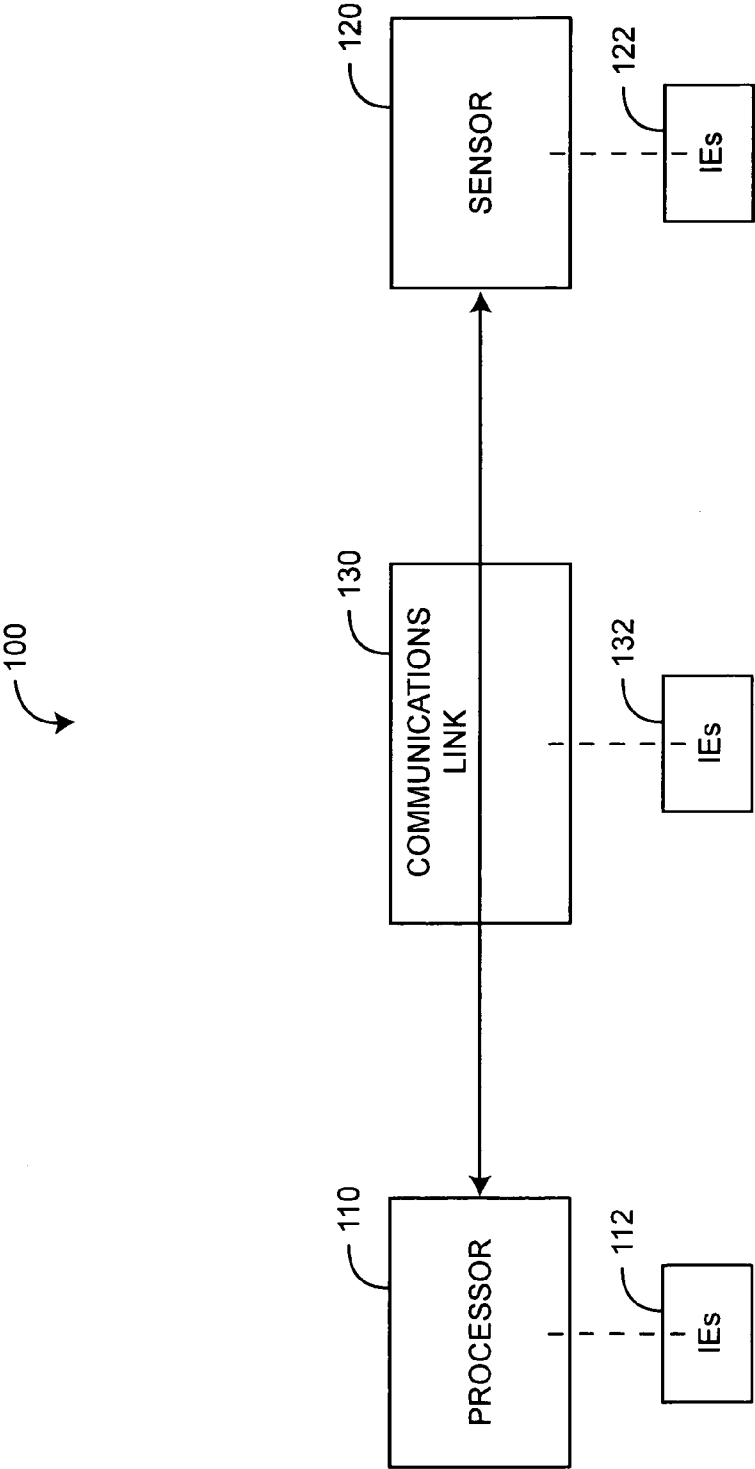


FIG. 1

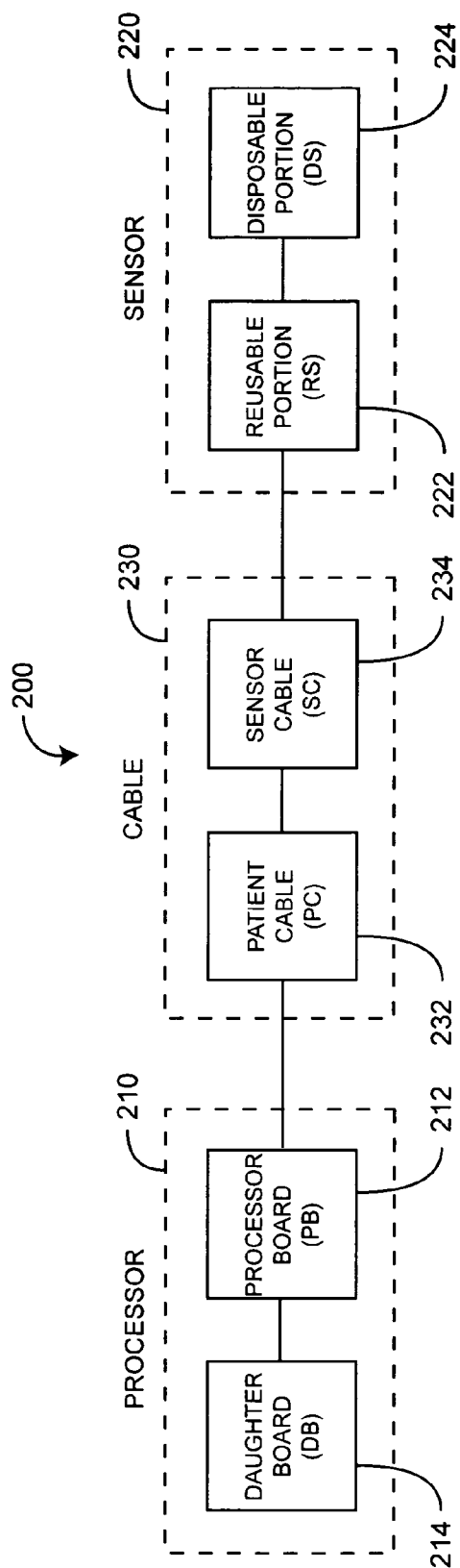


FIG. 2

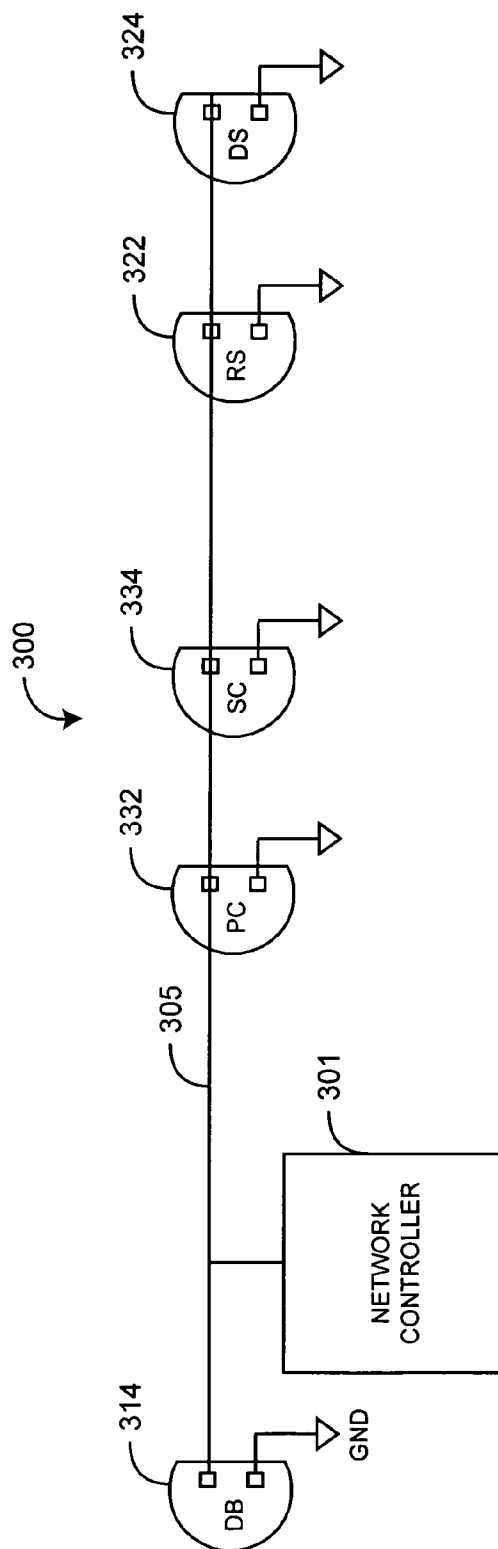


FIG. 3

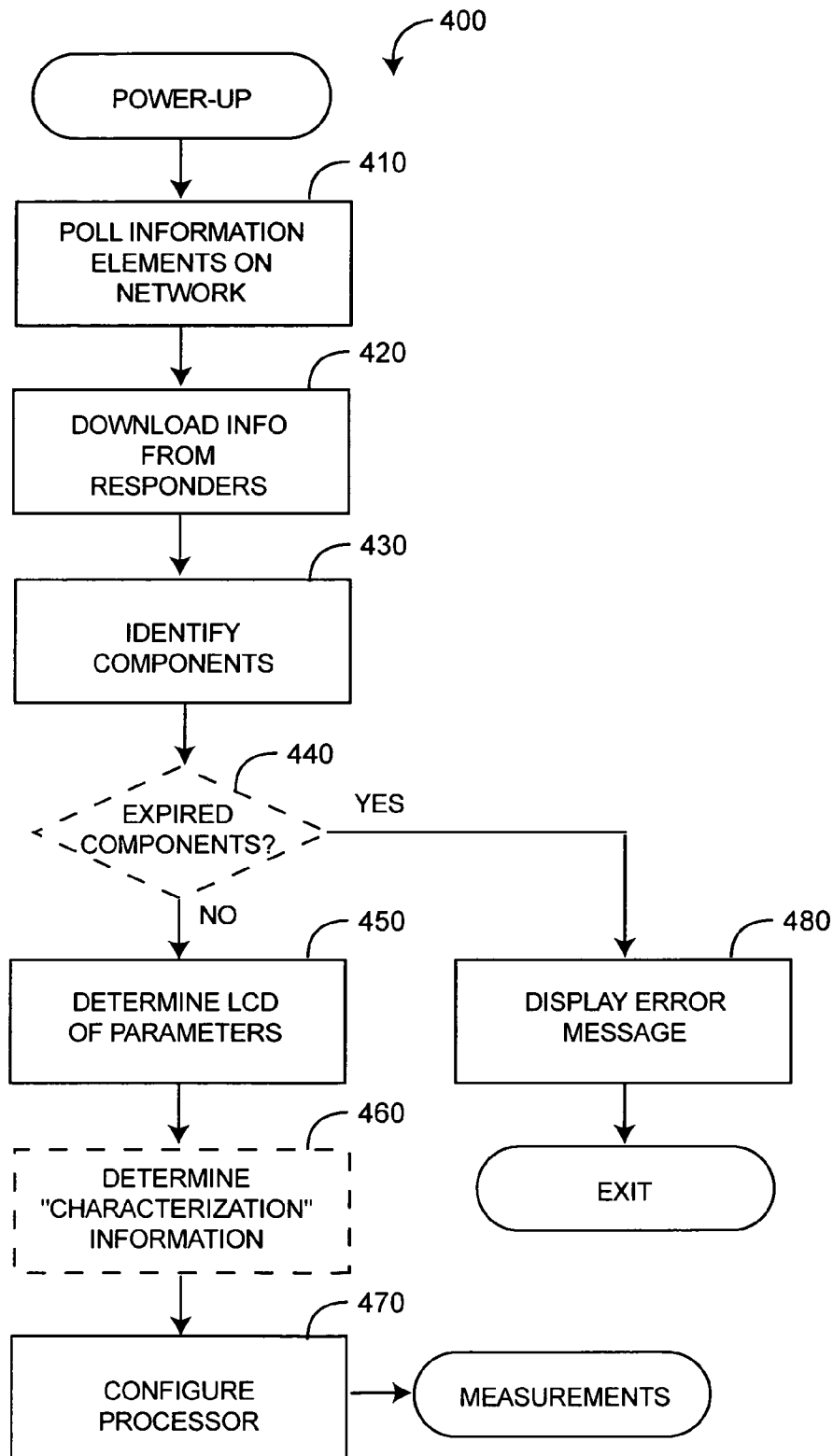


FIG. 4

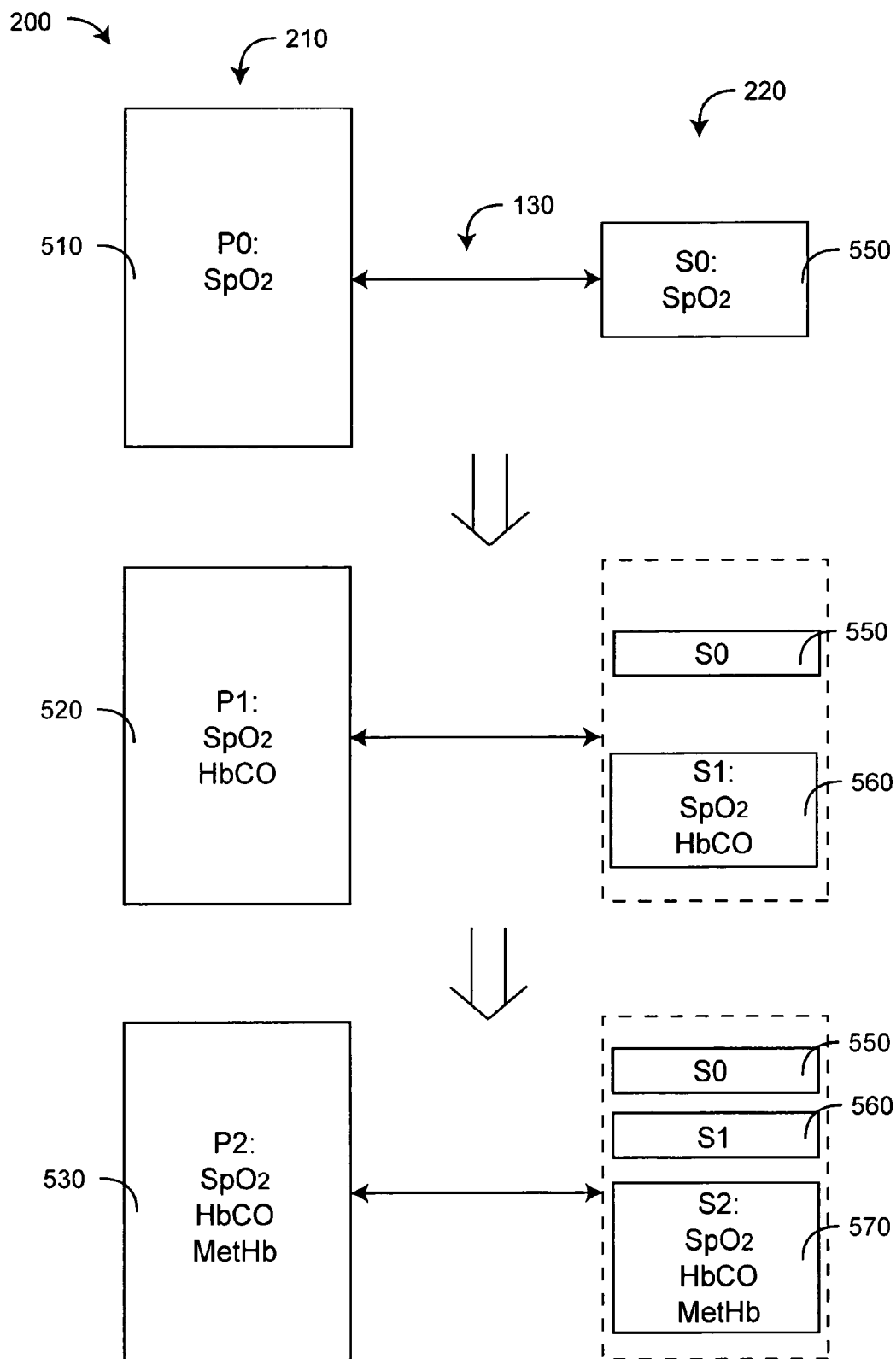


FIG. 5A

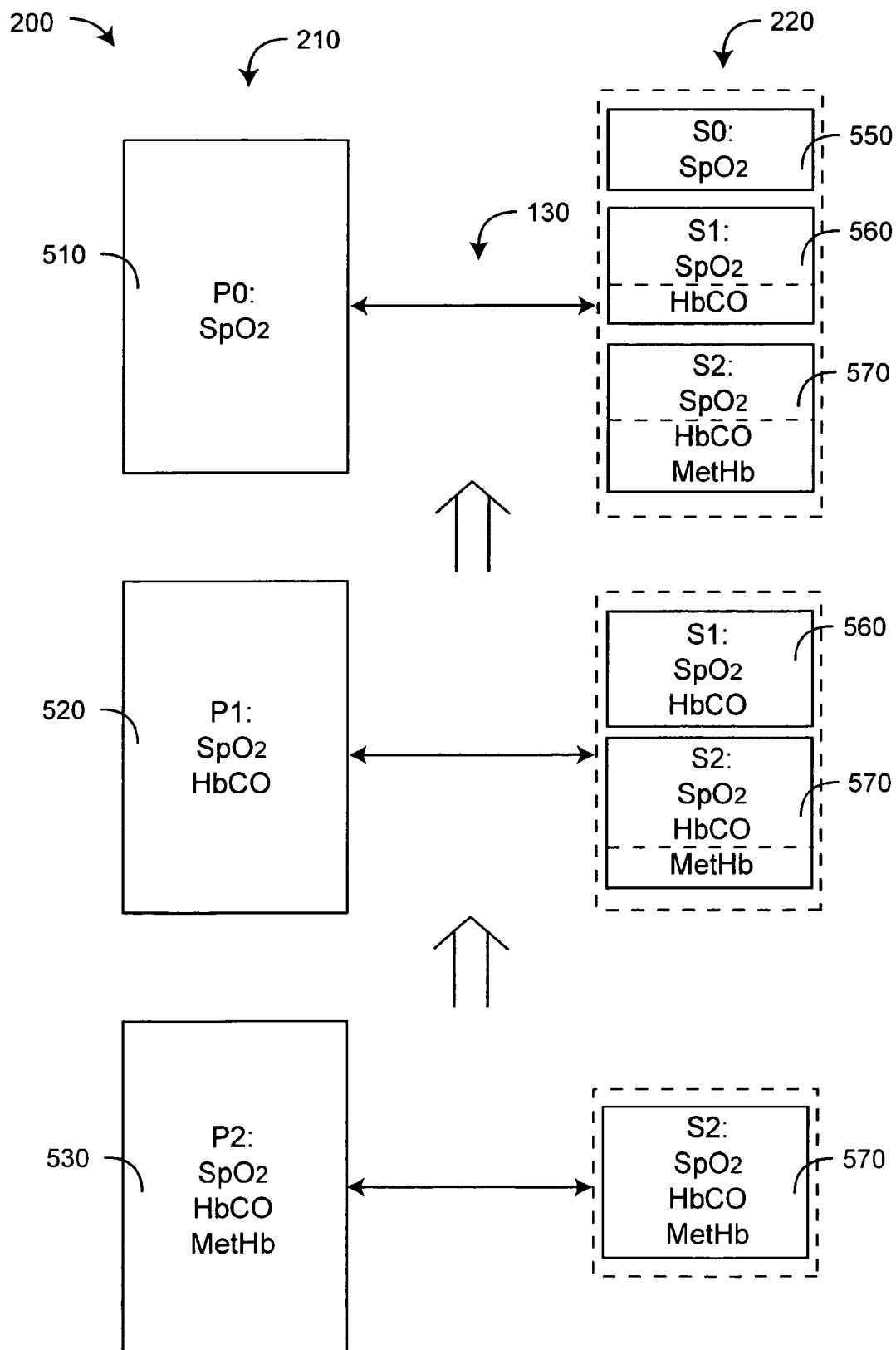


FIG. 5B

CONFIGURABLE PHYSIOLOGICAL MEASUREMENT SYSTEM

PRIORITY CLAIM TO RELATED PROVISIONAL APPLICATIONS

The present application claims priority benefit under 35 U.S.C. §119(e) to U.S. Provisional Patent Application Ser. No. 60/657,596, filed Mar. 1, 2005, entitled "Multiple Wavelength Sensor," No. 60/657,281, filed Mar. 1, 2005, entitled "Physiological Parameter Confidence Measure," No. 60/657,268, filed Mar. 1, 2005, entitled "Configurable Physiological Measurement System," and No. 60/657,759, filed Mar. 1, 2005, entitled "Noninvasive Multi-Parameter Patient Monitor." The present application incorporates the foregoing disclosures herein by reference.

INCORPORATION BY REFERENCE OF COPENING RELATED APPLICATIONS

The present application is related to the following copending U.S. utility applications:

	App. Sr. No.	Filing Date	Title	Atty Dock.
1	11/367,013	Mar. 1, 2006	Multiple Wavelength Sensor Emitters	MLR.002A
2	11/366,995	Mar. 1, 2006	Multiple Wavelength Sensor Equalization	MLR.003A
3	11/366,209	Mar. 1, 2006	Multiple Wavelength Sensor Substrate	MLR.004A
4	11/366,210	Mar. 1, 2006	Multiple Wavelength Sensor Interconnect	MLR.005A
5	11/366,833	Mar. 1, 2006	Multiple Wavelength Sensor Attachment	MLR.006A
6	11/366,997	Mar. 1, 2006	Multiple Wavelength Sensor Drivers	MLR.009A
7	11/367,034	Mar. 1, 2006	Physiological Parameter Confidence Measure	MLR.010A
8	11/367,036	Mar. 1, 2006	Configurable Physiological Measurement System	MLR.011A
9	11/367,033	Mar. 1, 2006	Noninvasive Multi-Parameter Patient Monitor	MLR.012A
10	11/367,014	Mar. 1, 2006	Noninvasive Multi-Parameter Patient Monitor	MLR.013A
11	11/366,208	Mar. 1, 2006	Noninvasive Multi-Parameter Patient Monitor	MLR.014A

The present application incorporates the foregoing disclosures herein by reference.

BACKGROUND OF THE INVENTION

Spectroscopy is a common technique for measuring the concentration of organic and some inorganic constituents of a solution. The theoretical basis of this technique is the Beer-Lambert law, which states that the concentration c_i of an absorbent in solution can be determined by the intensity of light transmitted through the solution, knowing the path-length d_λ , the intensity of the incident light $I_{0,\lambda}$, and the extinction coefficient $\epsilon_{i,\lambda}$, at a particular wavelength λ . In generalized form, the Beer-Lambert law is expressed as:

$$I_\lambda = I_{0,\lambda} e^{-d_\lambda \cdot \mu_{a,\lambda}} \quad (1)$$

$$\mu_{a,\lambda} = \sum_{i=1}^n \epsilon_{i,\lambda} \cdot c_i \quad (2)$$

where $\mu_{a,\lambda}$ is the bulk absorption coefficient and represents the probability of absorption per unit length. The minimum number of discrete wavelengths that are required to solve EQS. 1-2 are the number of significant absorbers that are present in the solution.

A practical application of this technique is pulse oximetry, which utilizes a noninvasive sensor to measure oxygen saturation (SpO_2) and pulse rate. In general, the sensor has light emitting diodes (LEDs) that transmit optical radiation of red and infrared wavelengths into a tissue site and a detector that responds to the intensity of the optical radiation after absorption (e.g., by transmission or transreflectance) by pulsatile arterial blood flowing within the tissue site. Based on this response, a processor determines measurements for SpO_2 , pulse rate, and can output representative plethysmographic waveforms. Thus, "pulse oximetry" as used herein encompasses its broad ordinary meaning known to one of skill in the art, which includes at least those noninvasive procedures for measuring parameters of circulating blood through spectroscopy. Moreover, "plethysmograph" as used herein (commonly referred to as "photoplethysmograph"), encompasses its broad ordinary meaning known to one of skill in the art, which includes at least data representative of a change in the absorption of particular wavelengths of light as a function of the changes in body tissue resulting from pulsing blood. Pulse oximeters capable of reading through motion induced noise are available from Masimo Corporation ("Masimo") of Irvine, Calif. Moreover, portable and other oximeters capable of reading through motion induced noise are disclosed in at least U.S. Pat. Nos. 6,770,028, 6,658,276, 6,157,850, 6,002,952, 5,769,785, and 5,758,644, which are owned by Masimo and are incorporated by reference herein. Such reading through motion oximeters have gained rapid acceptance in a wide variety of medical applications, including surgical wards, intensive care and neonatal units, general wards, home care, physical training, and virtually all types of monitoring scenarios.

SUMMARY OF THE INVENTION

A physiological measurement system has a sensor that transmits optical radiation at a multiplicity of wavelengths other than or including the red and infrared wavelengths utilized in pulse oximeters. The system also has a processor that determines the relative concentrations of blood constituents other than or in addition to HbO_2 and Hb, such as carboxyhemoglobin ($HbCO$), methemoglobin ($MetHb$), fractional oxygen saturation, total hemoglobin (Hbt) and blood glucose to name a few. Further, such a system may be combined with other physiological parameters such as noninvasive blood pressure (NIBP). There is a need to easily configure such a physiological measurement system from compatible components capable of measuring various physiological parameters.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a general block diagram of a configurable physiological measurement system;

FIG. 2 is a detailed block diagram of a configurable physiological measurement system embodiment;

FIG. 3 is a detailed block diagram of networked information elements in a configurable physiological measurement system;

FIG. 4 is a flowchart of a physiological measurement system configuration process; and

FIGS. 5A-B are block diagrams illustrating forward and backward sensor compatibility with various processors.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

In this application, reference is made to many blood parameters. Some references that have common shorthand designations are referenced through such shorthand designations. For example, as used herein, HbCO designates carboxyhemoglobin, HbMet designates methemoglobin, and Hbt designates total hemoglobin. Other shorthand designations such as COHb, MetHb, and tHb are also common in the art for these same constituents. These constituents are generally reported in terms of a percentage, often referred to as saturation, relative concentration or fractional saturation. Total hemoglobin is generally reported as a concentration in g/dL. The use of the particular shorthand designators presented in this application does not restrict the term to any particular manner in which the designated constituent is reported.

FIG. 1 illustrates a configurable physiological measurement system 100 having a processor 110, a sensor 120 and a communications link 130. In one embodiment, the sensor 120 has two or more light emitters that transmit optical radiation of two or more wavelengths into a tissue site and at least one detector that generates a signal responsive to the optical radiation after attenuation by the tissue site. Multiple wavelength sensors are described in U.S. patent application Ser. No. 10/719,928, entitled Blood Parameter Measurement System, assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

The processor 110 generates drive signals so as to activate the sensor emitters and inputs and processes the corresponding detector signal so as to determine the relative concentrations of two or more blood constituents. The communications link 130 provides communications between the processor 110 and sensor 120 including transmitting the drive signals from the processor 110 to the sensor 120 and the detector signals from the sensor 120 to the processor 110. In one embodiment, the communications link 130 is a cable and corresponding sensor and processor connectors that provide a wired connection between the processor 110 and connector 120. In another embodiment, the communications link 130 provides a wireless connection between the processor 110 and connector 120. The wireless connection may utilize Bluetooth®, IEEE 802.11 or similar wireless technologies.

As shown in FIG. 1, the configurable physiological measurement system 100 also has information elements 112, 122, 132 distributed across the processor 110, the sensor 120 and the communications link 130, which provide system configuration information, as described below. The information elements 112, 122, 132 may be memory devices, such as described below, or other active or passive electrical components. The information provided by the information elements 112, 122, 132 may be digital data stored in memory or component values determined by DC, AC or combinations of DC and AC voltages or currents. The information element 112, 122, 132 information may be determined by the processor 110 or by a reader or other device in communication with the information elements 112, 122, 132 and the processor 110.

FIG. 2 illustrates configurable physiological measurement system embodiments having processor 210, sensor 220 and cable 230 components. In one embodiment, the processor 210 has a processor printed circuit board "board" 212 and an optional daughter board 214, which plugs into and expands the functionality of the processor board 212. For example, the daughter board 214 may be a noninvasive blood pressure

(NIBP) controller that communicates with a blood pressure sensor and the processor board 212 so as to measure blood pressure parameters.

Also shown in FIG. 2, in one embodiment the sensor 220 is a "resposable" sensor comprising a reusable portion 222 and a disposable portion 224. In a particular embodiment, the reusable portion has at least one of a reusable emitter portion and a reusable detector portion, and the disposable portion 224 has at least one of a disposable emitter portion, a disposable detector portion and a disposable tape for attaching the reusable sensor 222 to a tissue site. A resposable sensor is described in U.S. Pat. No. 6,725,075 entitled Resposable Pulse Oximetry Sensor, assigned to Masimo Corporation and incorporated by reference herein.

Further shown in FIG. 2, in one embodiment the cable 230 is a patient cable 232 or a sensor cable 234 or a combination of a patient cable 232 and a sensor cable 234. A sensor cable 234 is fixedly attached at one end to a sensor and has a connector at the other end for attaching to a monitor or a patient cable. A patient cable 234 has connectors at both ends for interconnecting a sensor or sensor cable to a monitor.

FIG. 3 illustrates an information element (IE) network 300 that advantageously enables a physiological measurement system 200 (FIG. 2) to be composed of various components 214-234 (FIG. 2) having, perhaps, differing parameter measurement capabilities, as described above. The IE network 300 also allows various components to "plug and play," i.e. interoperate without hardware or software modification, as described with respect to FIG. 4, below. Further, the IE network 300 provides for forward and backward compatibility between sensors and processors, as described with respect to FIGS. 5A-B, below.

As shown in FIG. 3, the IE network 300 has information elements 314-334, a network controller 301 and a communications path 305. In one embodiment, the network controller 301 resides on or is otherwise incorporated within a processor board 212 (FIG. 2). The information elements 314-334 correspond to the physiological measurement system components 210-230 (FIG. 2). In one embodiment, there may be zero, one, two or more information elements 314-334 on or within each physiological measurement system component 214-224 (FIG. 2). For example, the information elements 314-324 may include a DB element 314 mounted on a daughter board 214 (FIG. 2), a RS element 322 mounted within a reusable sensor portion 222 (FIG. 2), a DS element 324 mounted within a disposable sensor portion 224 (FIG. 2), a PC element 332 mounted within a patient cable 232 (FIG. 2) or connector thereof, and a SC element 334 mounted within a sensor cable 234 (FIG. 2) or connector thereof.

Also shown in FIG. 3, in one embodiment the information elements 314-334 are EPROMs or EEPROMs or a combination of EPROMs or EEPROMs within a particular component 210-230 (FIG. 2). In an advantageous embodiment, the communications path 305 is a single shared wire. This reduces the burden on the components 210-230 (FIG. 2) and associated connectors, which may have a relatively large number of conductors just for drive signals and detector signals when a multiplicity of sensor emitters are utilized for multiple parameter measurements. An information element 314-324 may be, for example, a Dallas Semiconductor DS2506 EPROM available from Maxim Integrated Products, Inc., Sunnyvale, Calif., or equivalent.

FIG. 4 illustrates a configuration process 400 for a physiological measurement system 200 (FIG. 2). This process is executed by the network controller 301 (FIG. 3) or the processor 210 (FIG. 2) or both with respect to information elements 314-334 (FIG. 3) that exist on the network 305 (FIG.

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3). After system power-up, any information elements on the network are polled **410** so they identify themselves. Information is then downloaded from the responding information elements **420**. In one embodiment, download information can be some or all of Identification (ID), Life, Parameters, Characterization and Features information. ID identifies a component on the network, either the type of component generally, such as a sensor or cable, or a particular part number, model and serial number, to name a few. As another example, ID for a disposable sensor portion **224** (FIG. 2) may be an attachment location on a patient and ID for a reusable sensor portion **222** (FIG. 2) may be a patient type.

Life, for example, may be a predetermined counter written into an EEPROM to indicate the number of uses or the length of use of a particular component. Then, Life is counted down, say each time power is applied, until a zero value is reached, indicating component expiration.

Parameters specifies the measurements the component is capable of supporting, which may include, for example, one or more of SpO₂, HbCO, MetHb, fractional SpO₂, Hbt, NIBP and blood glucose to name just a few. With respect to a sensor, Parameters depend on the number of emitters, emitter wavelength and emitter configuration, for example. For a cable, Parameters depend on the number of conductors and connector pinouts, for example. Parameters may also simply reflect a license to use a component, such as disposable tape, with respect to a particular system configuration.

Features set the mode for the processor or other system elements. As one example, Features specify the mode or modes of one or more algorithms, such as averaging.

Characterization allows the processor to “plug and play” with a particular component. For example, if the component is a sensor, Characterization may include information necessary to drive the emitters, such as the LED wavelengths and drive pattern. Characterization may also include calibration data for the parameters measured. As another example, Characterization for a sensor component **220** (FIG. 2) may indicate sensitivity to a probe-off condition depending on the sensor type. Probe-off detection is described in U.S. Pat. No. 6,654,624 entitled Pulse Oximeter Probe-Off Detector and U.S. Pat. No. 6,771,994 entitled Pulse Oximeter Probe-Off Detection System, both assigned to Masimo Corporation and incorporated by reference herein.

As shown in FIG. 4, components are identified **430** from downloaded ID information. If any of the information elements provide Life information, a check is made to determine if the corresponding component is expired **440**. If so, an error message is displayed **480**. The message may be a warning to replace the component or it may indicate that the system is nonfunctional. Next, the least common denominator (LCD) of the parameters is determined **450** from the Parameters information. This is described in further detail with respect to FIGS. 5A-B. Characterization is determined **460**, if necessary for a particular component, such as a daughterboard or sensor. Finally, the processor is configured **470** and the system is ready to begin parameter measurements.

FIGS. 5A-B illustrate embodiments of a configurable physiological measurement system **100** demonstrating both forward sensor compatibility (FIG. 5A), and backward sensor compatibility (FIG. 5B). Further, the parameter measurement capability of each system **100** is determined by the least common denominator (LCD) of the parameter capabilities of a processor **210** and a sensor **220**.

As shown in FIG. 5A, configurable physiological measurement systems **200** comprise a family of processors (P0, P1, P2) **210** including those capable of computing SpO₂ **510-530**, HbCO **520-530** and MetHb **530**. The systems **200** also comprise a family of sensors **220** (S0, S1, S2) including those capable of detecting SpO₂ **550-570**, HbCO **560-570** and

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MetHb **570**. Here, the lower numbered processors and sensors represent less capability, e.g. older generation processors and sensors or current generation, but less costly processors and sensors. Illustrated is forward sensor compatibility, i.e. less capable sensors are capable of running on more capable processors. For example, an SpO₂ only sensor **550** is capable of working with a multiple parameter (SoO₂, HbCO, MetHb) processor **530**. Also illustrated is LCD functionality. A system **200** having a P2 processor **530** and a S0 sensor **550** is functional but only capable of measuring SpO₂.

FIG. 5B illustrates backward sensor compatibility, i.e. more capable sensors are capable of running on less capable processors. For example, a multiple parameter (SpO₂, HbCO, MetHb) sensor **570** is capable of working with an SpO₂ only processor **510**. Also, a system **200** having a P0 processor **510** and a S2 sensor **570** is functional, but only capable of measuring SpO₂.

Forward and backward sensor compatibility is described above with respect to configurable physiological measurement systems **200** having various processor **210** capabilities and sensor **220** capabilities. The configurable physiological measurement systems **200** can have any or all of the processor **210**, sensor **220** and cable **230** components described with respect to FIG. 2, above. As such forward and backward compatibility is equally applicable to combinations of processor **210** and cable **230** or combinations of sensor **220** and cable **230**, including the components of such described with respect to FIG. 2, where the capability of such combinations is determined by LCD functionality, as described above.

A configurable physiological measurement system has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

What is claimed is:

1. A physiological measurement system comprising:
 - a sensor configured to transmit light having a plurality of wavelengths into a tissue site and to generate a sensor signal responsive to the transmitted light after tissue attenuation;
 - a processor configured to operate on the sensor signal so as to derive at least one physiological parameter;
 - a communications link adapted to provide communications between the sensor and the processor; and
 - a plurality of information elements distributed across at least one of the sensor, the processor and the communications link,
 wherein the information elements provide operational information corresponding to at least one of the sensor, the processor and the communications link, the processor configured to determine a least common denominator of parameter measurement capabilities based on the operational information.
2. The physiological measurement system according to claim 1 further comprising a network controller capable of reading the information elements and providing the information to the processor.
3. The physiological measurement system according to claim 1 wherein the sensor comprises a reusable portion and a disposable portion, each having at least one of the information elements.
4. The physiological measurement system according to claim 3 further comprising:
 - attachment data provided by a first information element associated with the disposable portion describing where the sensor is attached; and

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patient data provided by a second information element associated with the reusable portion describing patient type.

5. The physiological measurement system according to claim 1 further comprising:

at least one sensor information element associated with the sensor; and

sensor type data readable from the sensor information element,

wherein the processor utilizes the sensor type data to determine a sensitivity to a probe-off condition where the sensor is not properly positioned with respect to the tissue site.

6. A physiological measurement system comprising:

a sensor configured to transmit light having a plurality of wavelengths into a tissue site and to generate a sensor signal responsive to the transmitted light after tissue attenuation;

a processor configured to operate on the sensor signal so as to derive at least one physiological parameter;

a communications link adapted to provide communications between the sensor and the processor; and

a plurality of information elements distributed across at least one of the sensor, the processor and the communications link,

wherein the information elements provide operational information corresponding to at least one of the sensor, the processor and the communications link and wherein the processor comprises a processor board and a daughter board, each having at least one of the information elements.

7. The physiological measurement system according to claim 6 wherein the communications link is a cable having a patient cable portion and a sensor cable portion, each portion having at least one of the information elements.

8. In a physiological measurement system, a sensor configured to transmit light having a plurality of wavelengths into a tissue site and to generate a sensor signal responsive to the transmitted light after tissue attenuation, a processor configured to operate on the sensor signal so as to derive at least one physiological parameter and a communications link adapted to provide communications between the sensor and the processor, the sensor comprising:

a disposable portion of the sensor having a first information element; and

a reusable portion of the sensor having a second information element,

wherein the disposable portion is capable of removable attachment to the reusable portion, and

wherein the first information element and the second information are readable by the processor so as to determine the operational capability of the sensor and wherein the processor is configured to determine a least common denominator of parameter measurement capabilities.

9. The sensor according to claim 8 further comprising parameter information associated with at least one of the first information element and the second information element indicating physiological parameter measurements supported by at least one of the disposable portion, the reusable portion and the combination of the disposable portion and the reusable portion.

10. The sensor according to claim 9 wherein the parameter information comprises information relating to characteristics of light emitters incorporated on at least one of the disposable portion and the reusable portion.

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11. The sensor according to claim 8 further comprising: attachment information associated with the first information element describing where on a patient the sensor is attached; and

patient information associated with the second information element describing a patient type.

12. The sensor according to claim 8 further comprising sensor life information associated with the first information element that is updated according to a sensor usage measure.

13. The sensor according to claim 8 further comprising characterization information associated with at least one of the first information element and the second information element indicating at least one of light emitter wavelengths, light emitter drive requirements and calibration data.

14. A physiological measurement method for a system having a sensor configured to transmit light having a plurality of wavelengths into a tissue site, a processor configured to operate on a sensor signal responsive to the transmitted light after tissue attenuation and a communications link configured to provide communications between the sensor and the processor comprising the steps of:

reading a plurality of information elements distributed among at least one of the sensor, the processor and the communications link;

identifying components of the system based upon data read from the information elements;

determining a physiological parameter that the system is capable of measuring by determining a least common denominator of parameter measurement capabilities of the identified system components; and

configuring the processor to measure the physiological parameter.

15. The physiological measurement method according to claim 14 comprising the further step of characterizing at least one of the system components based upon data read from the information elements.

16. The physiological measurement method according to claim 15 comprising the further step of determining if any of the system components are expired.

17. The physiological measurement method according to claim 16 wherein the reading step comprises the substeps of: polling memory devices connected to a network; and downloading information from responding memory devices.

18. A physiological measurement system having sensor, communication and processor components configured to derive at least one physiological parameter based upon light having a plurality of wavelengths transmitted into a tissue site and detected after tissue attenuation, the physiological measurement system comprising an information element network means for allowing various configurations of the components to interoperate without modification, wherein the information element network means provides operational information and the processor component is configured to determine a least common denominator of parameter measurement capabilities based on the operational information.

19. The physiological measurement system according to claim 18 wherein the information element network means comprises a network controller means for reading data from individual information elements of the network.

20. The physiological measurement system according to claim 19 wherein the network controller means comprises a parameter means for determining the parameter measurement capability of the combined system components.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 7,729,733 B2
APPLICATION NO. : 11/367036
DATED : June 1, 2010
INVENTOR(S) : Al-Ali et al.

Page 1 of 1

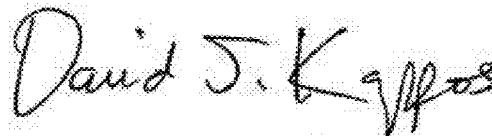
It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At column 1, line 60 (approx.), change " $\epsilon_{i,\lambda}$," to $-\epsilon_{i,\lambda}$.

At column 2, line 1, change " $\mu_{a,\lambda}$ " to $-\mu_{a,\lambda}$.

At column 6, line 7, change " SoO_2 ," to $-\text{SpO}_2$.

Signed and Sealed this
Twenty-eighth Day of December, 2010

A handwritten signature in black ink, reading "David J. Kappos". The signature is written in a cursive, flowing style with a large initial "D".

David J. Kappos
Director of the United States Patent and Trademark Office