

## US010524684B2

US 10,524,684 B2

Jan. 7, 2020

# (12) United States Patent

Fay et al.

(54)

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(10) Patent No.:

(45) **Date of Patent:** 

## USING MINI-ELECTRODES

TISSUE DIAGNOSIS AND TREATMENT

71) Applicant: Boston Scientific Scimed Inc., Maple

Grove, MN (US)

(72) Inventors: Leon Fay, Lexington, MA (US); Paul

Hultz, Brookline, MA (US)

(73) Assignee: Boston Scientific Scimed Inc, Maple

Grove, MN (US)

(\*) Notice: Subject to any disclaimer, the term of this

patent is extended or adjusted under 35

U.S.C. 154(b) by 557 days.

(21) Appl. No.: 14/881,112

(22) Filed: Oct. 12, 2015

(65) Prior Publication Data

US 2016/0100884 A1 Apr. 14, 2016

## Related U.S. Application Data

- (60) Provisional application No. 62/063,296, filed on Oct. 13, 2014.
- (51) Int. Cl.

  A61B 5/053 (2006.01)

  A61B 18/14 (2006.01)

  (Continued)
- (58) Field of Classification Search CPC ....... A61B 5/0422; A61B 2562/0257; A61B 2018/1497; A61B 2018/00892;

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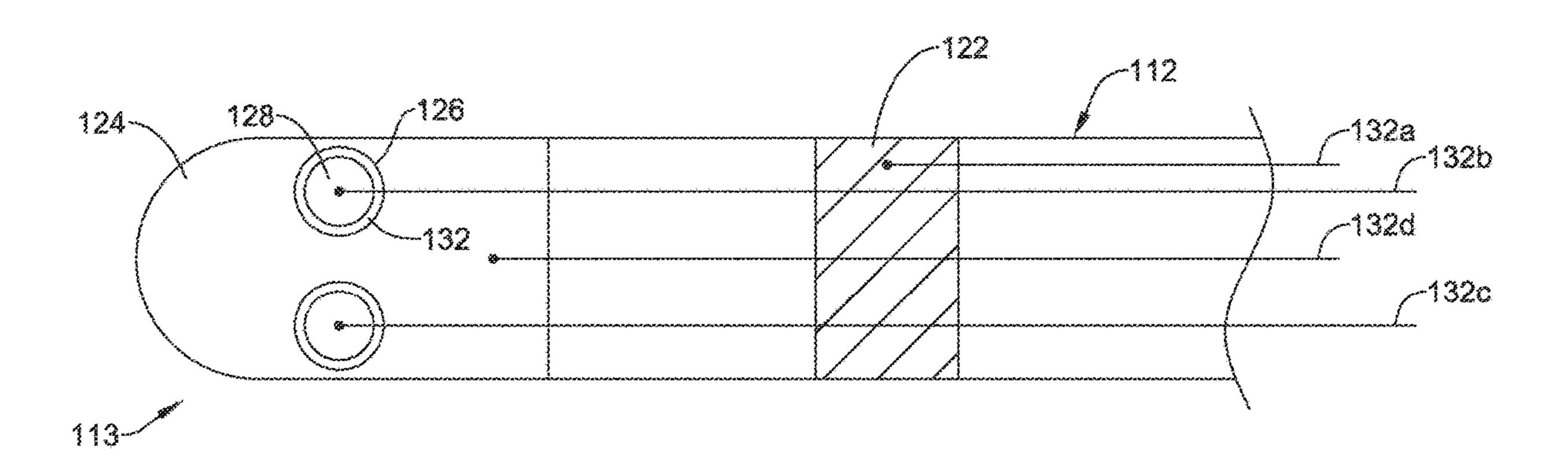
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Primary Examiner — Eun Hwa Kim (74) Attorney, Agent, or Firm — Faegre Baker Daniels LLP

## (57) ABSTRACT

Medical devices and methods for making and using medical devices are disclosed. An example electrophysiology medical device may include a catheter shaft including a distal end portion and a sensing assembly having three or more terminals. The sensing assembly includes one or more current-carrying electrodes and one or more sensing electrodes. The one or more current-carrying electrodes, the one or more sensing electrodes, or both includes a mini-electrode. The mini-electrode is disposed on one of the other electrodes. The medical device may also include a controller coupled to the sensing assembly.

## 19 Claims, 10 Drawing Sheets



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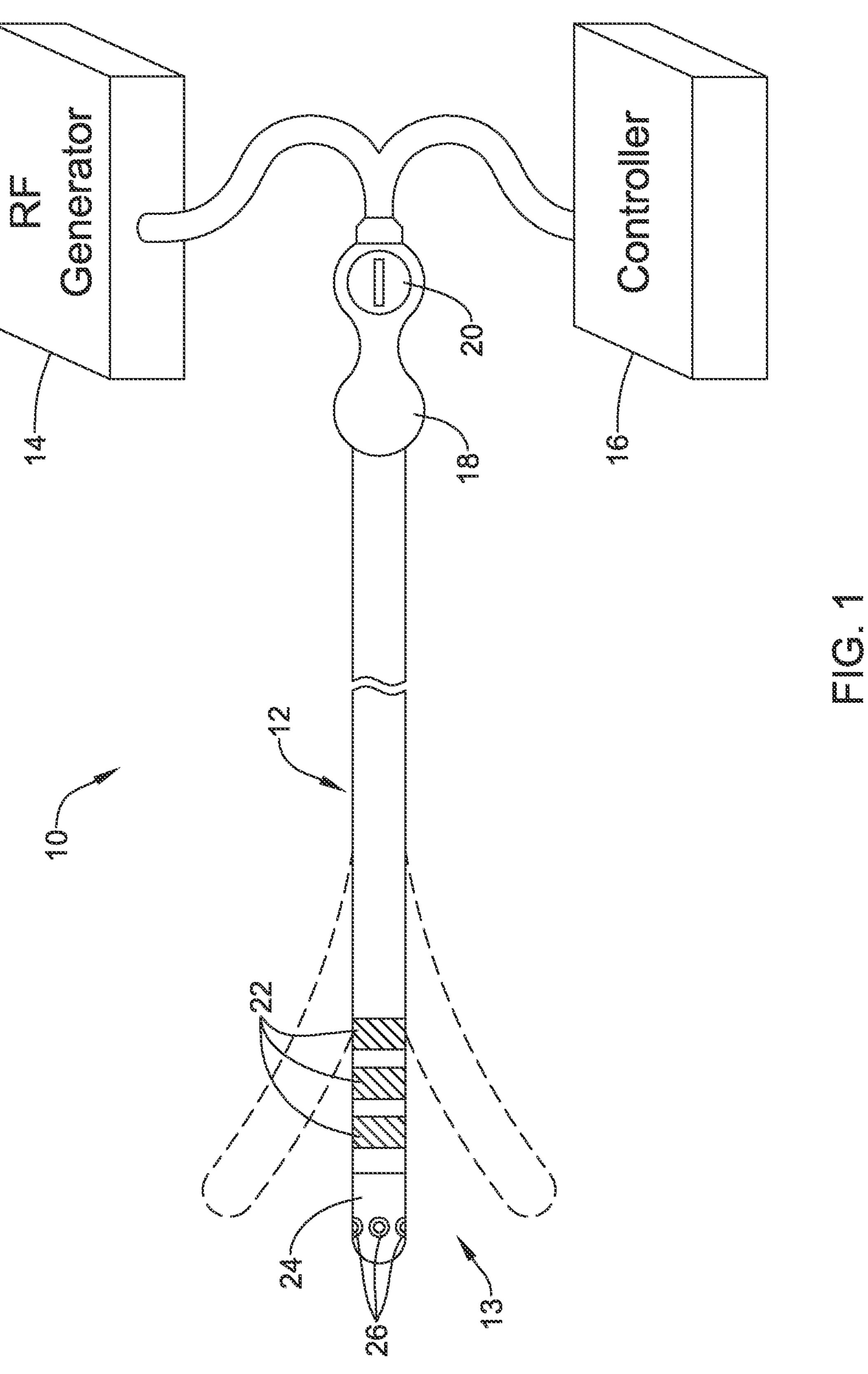
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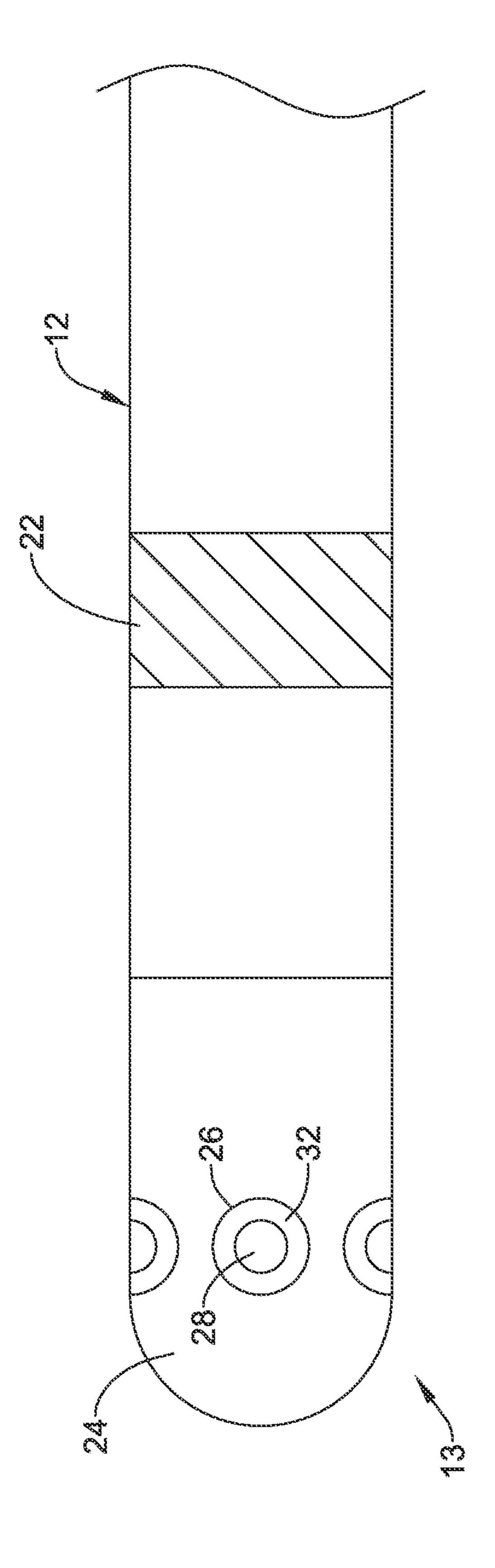
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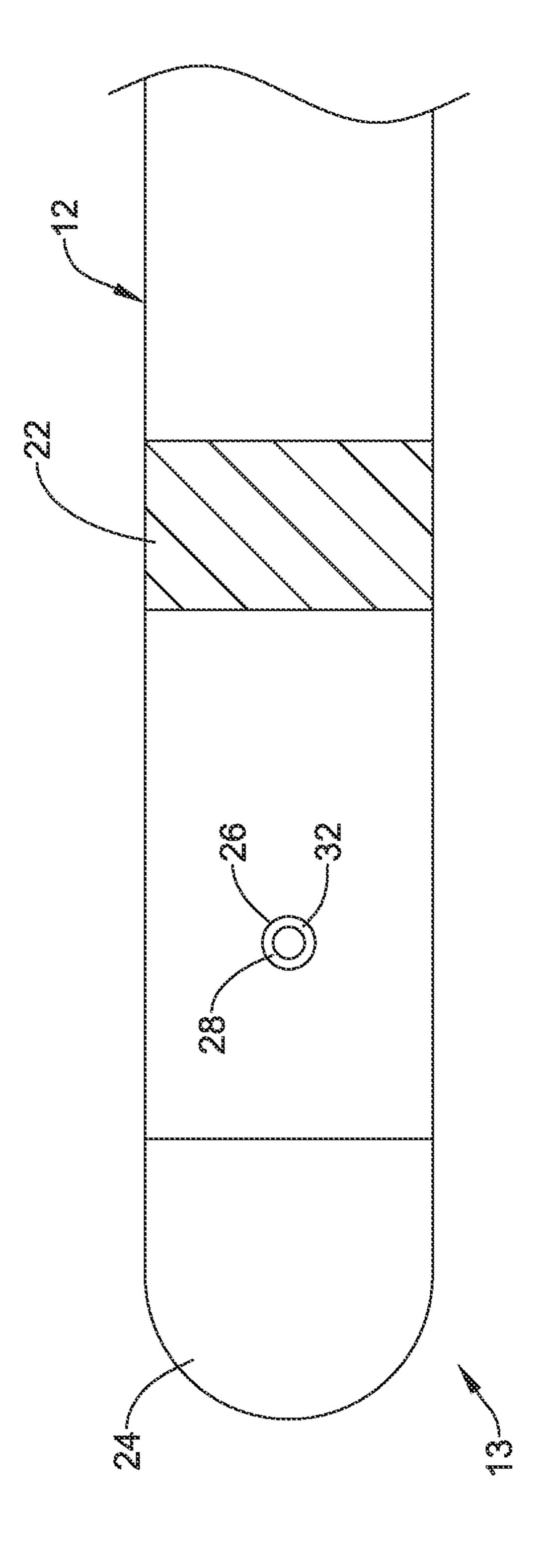
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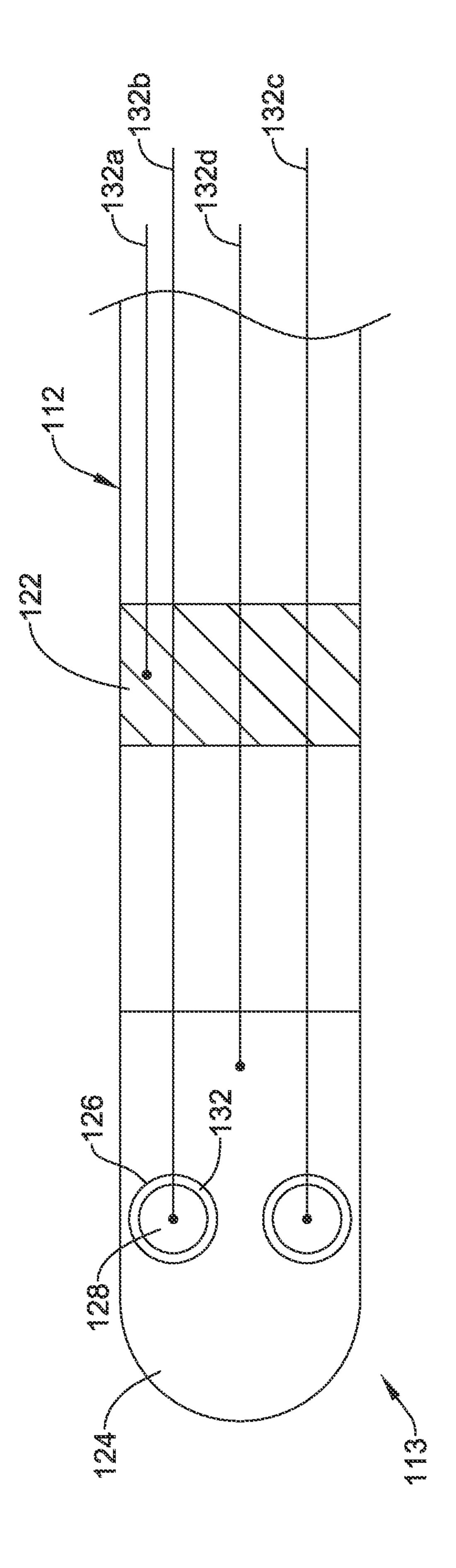
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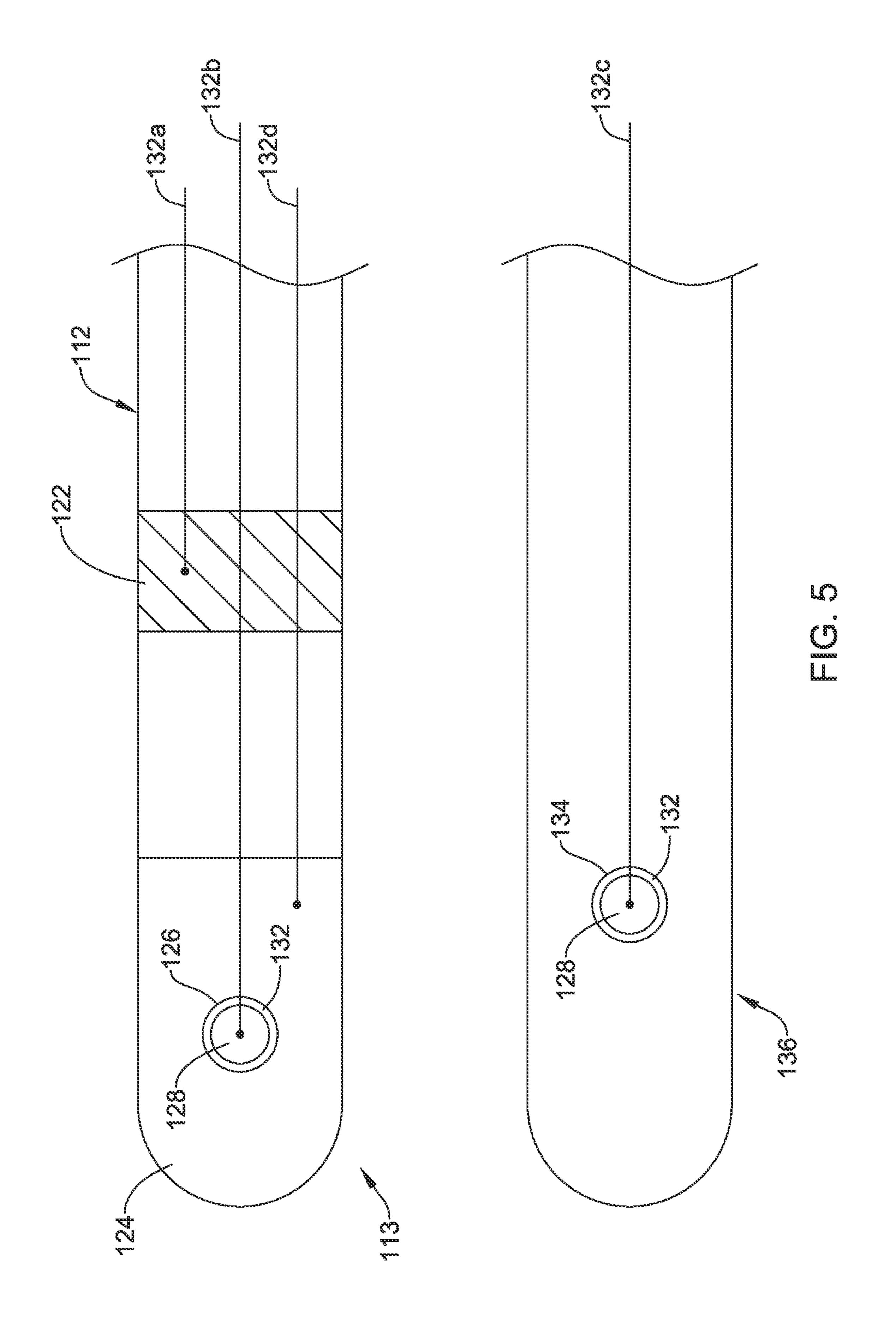
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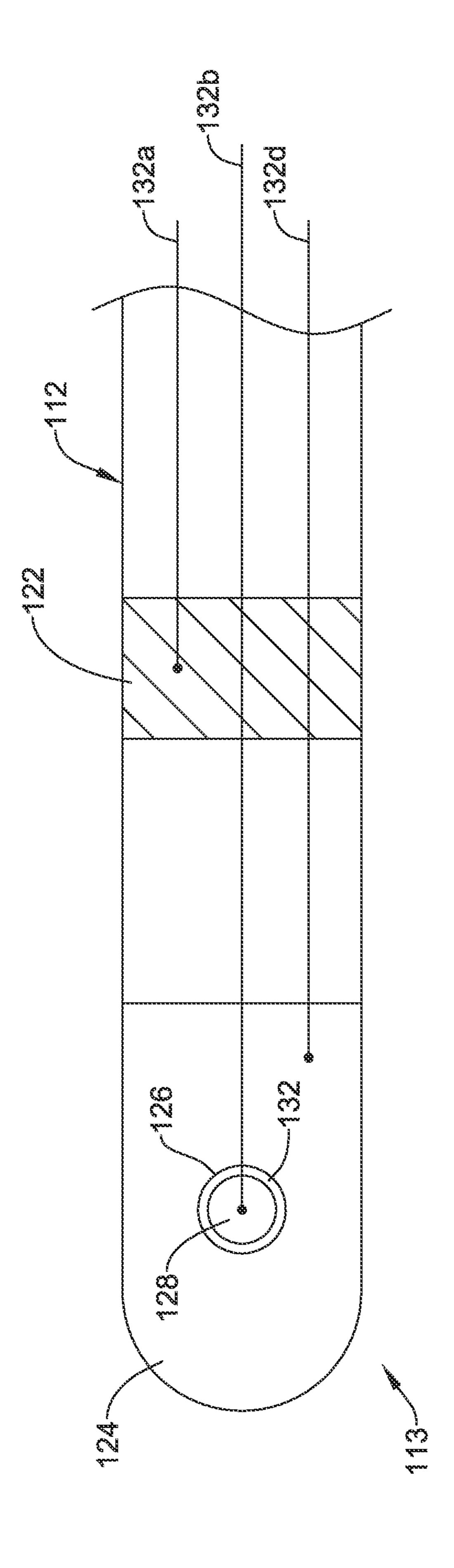


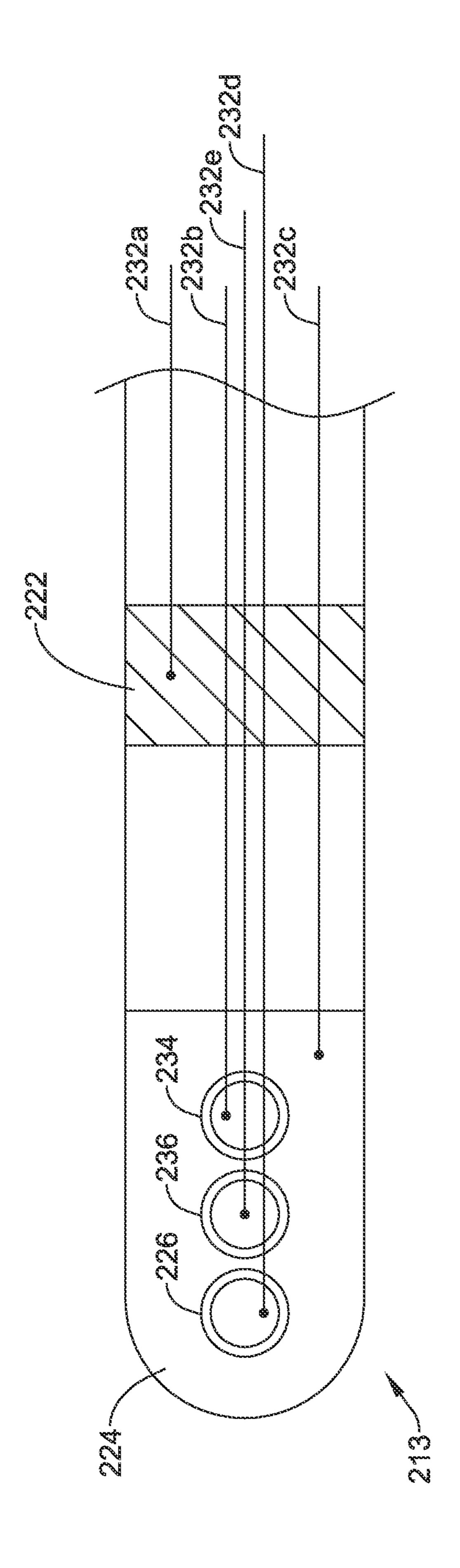


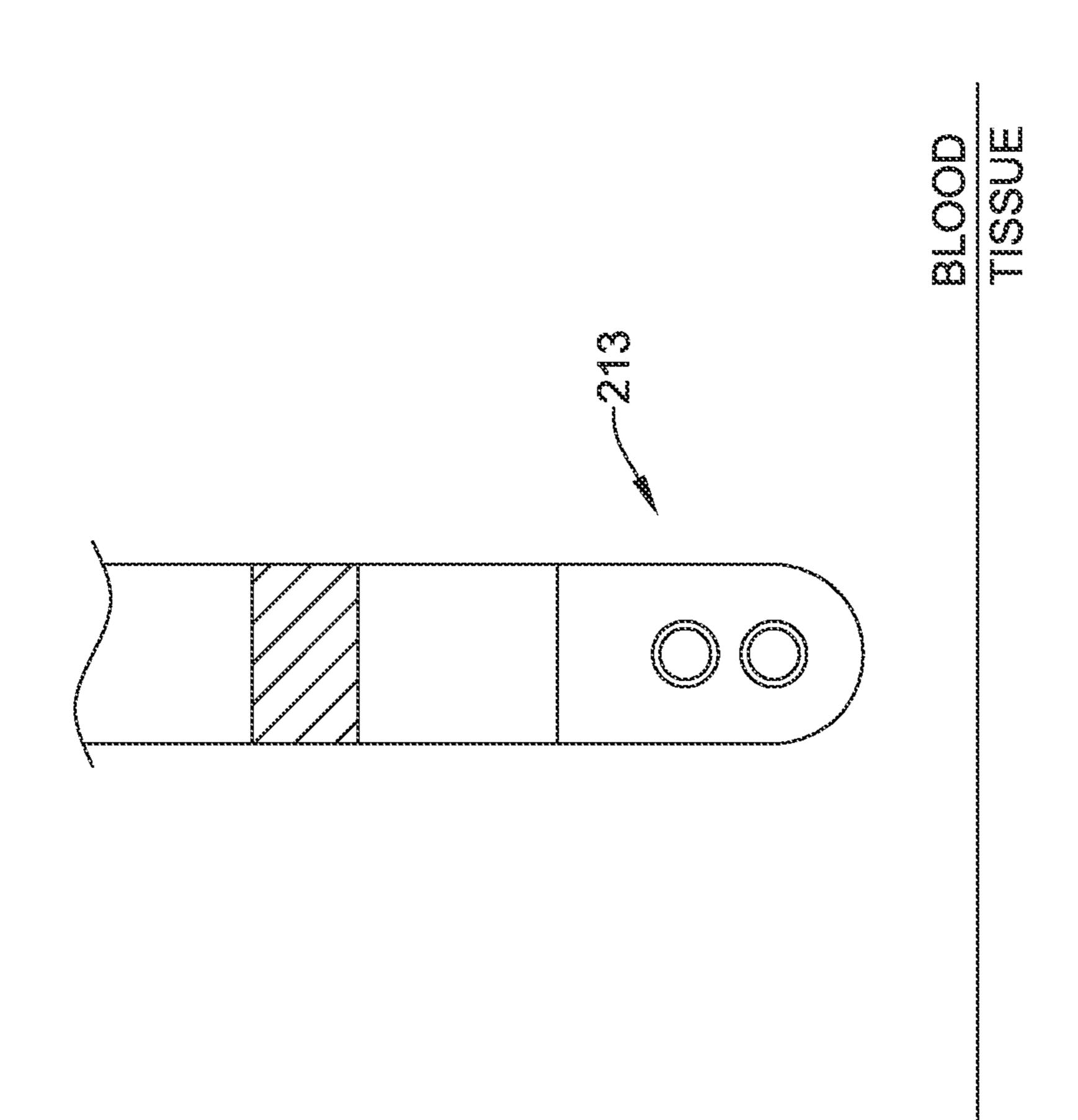


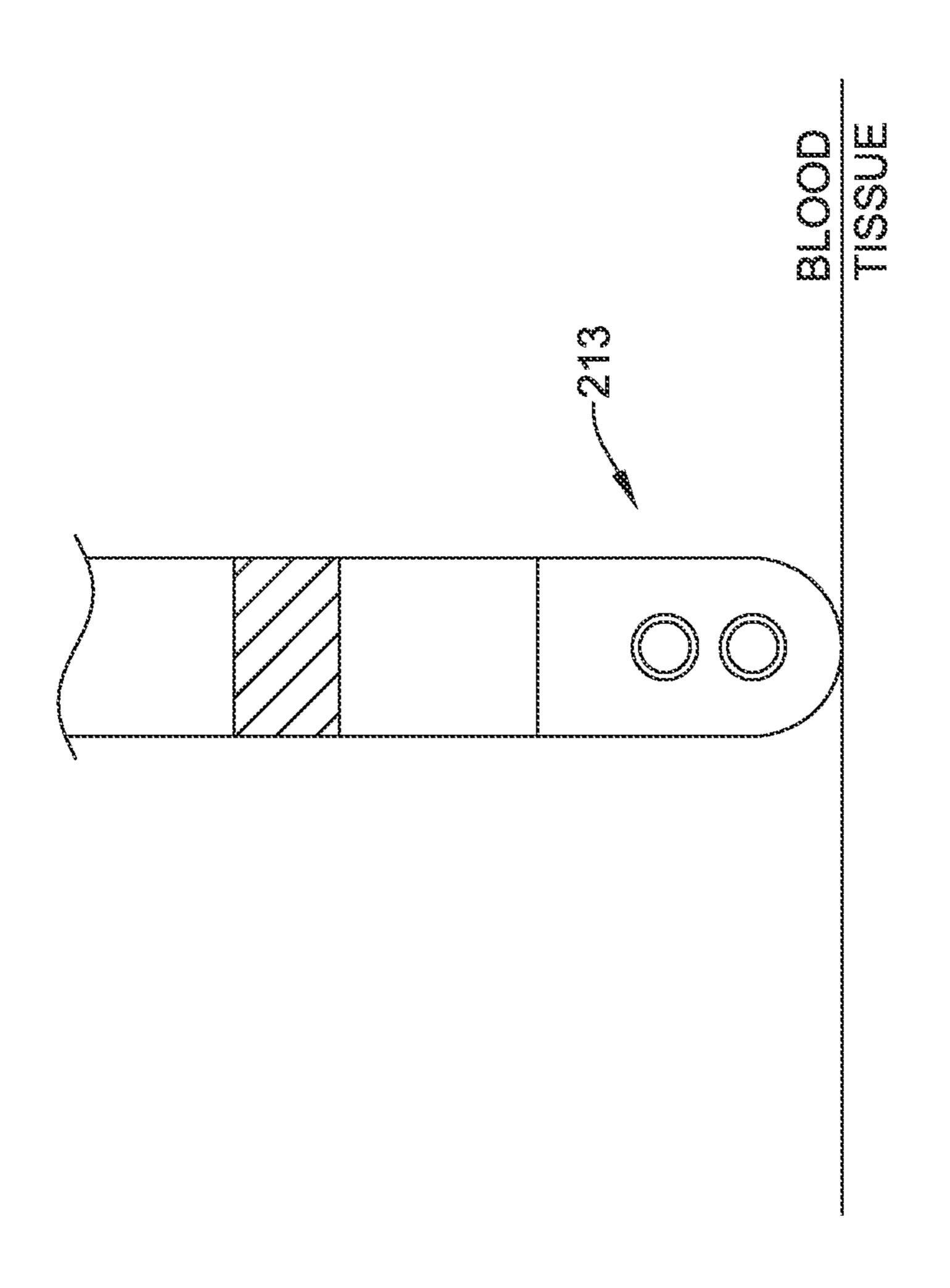


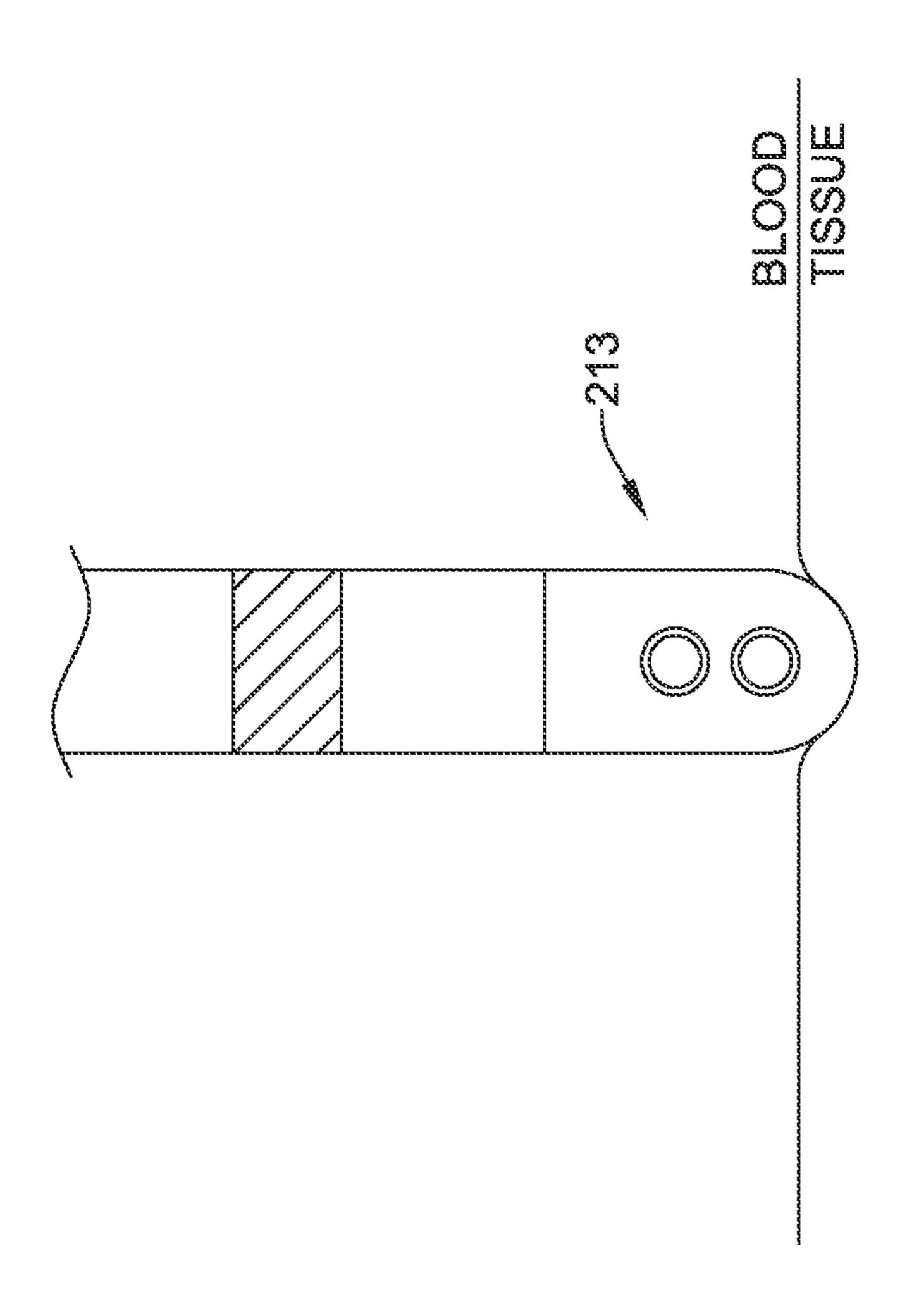












## TISSUE DIAGNOSIS AND TREATMENT USING MINI-ELECTRODES

## CROSS-REFERENCE TO RELATED APPLICATION

This application claims priority to Provisional Application No. 62/063,296, filed Oct. 13, 2014, which is herein incorporated by reference in its entirety.

### TECHNICAL FIELD

The present disclosure pertains to medical devices, and methods for manufacturing medical devices. More particularly, the present disclosure pertains to tissue diagnosis and/or ablation.

## **BACKGROUND**

A wide variety of intracorporeal medical devices have been developed for medical use, for example, intravascular <sup>20</sup> use. Some of these devices include guidewires, catheters, and the like. These devices are manufactured by any one of a variety of different manufacturing methods and may be used according to any one of a variety of methods. Of the known medical devices and methods, each has certain <sup>25</sup> advantages and disadvantages. There is an ongoing need to provide alternative medical devices as well as alternative methods for manufacturing and using medical devices.

## **SUMMARY**

This disclosure provides design, material, manufacturing method, and use alternatives for medical devices. An example electrophysiology medical device may include a catheter shaft including a distal end portion and a sensing assembly having three or more terminals. The sensing assembly includes one or more current-carrying electrodes and one or more sensing electrodes. The one or more current-carrying electrodes, or both includes a mini-electrode. The mini-electrode 40 is disposed on one of the other electrodes. The medical device may also include a controller coupled to the sensing assembly.

Additionally or alternatively to any of the examples above, the sensing assembly includes four terminals.

Additionally or alternatively to any of the examples above, one or more of the three or more terminals are disposed along the distal end portion of the catheter shaft.

Additionally or alternatively to any of the examples above, one or more of the three or more terminals are 50 disposed along a device separate from the catheter shaft.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes at least one mini-electrode.

Additionally or alternatively to any of the examples 55 above, one or more current-carrying electrodes includes at least two mini-electrodes.

Additionally or alternatively to any of the examples above, one or more sensing electrodes includes one mini-electrode.

Additionally or alternatively to any of the examples above, one or more sensing electrodes includes two minielectrodes.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes a 65 mini-electrode and one or more sensing electrodes includes two mini-electrodes.

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Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes two mini-electrodes and one or more sensing electrodes includes a mini-electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes two mini-electrodes and one or more sensing electrodes includes two mini-electrodes.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes or one or more sensing electrodes includes an ablation electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes an ablation electrode and one or more sensing electrodes includes an electrode disposed on the ablation electrode.

Additionally or alternatively to any of the examples above, one or more sensing electrodes includes an ablation electrode and one or more current-carrying electrodes includes an electrode disposed on the ablation electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes or one or more sensing electrodes includes a ring electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes an ablation electrode and a ring electrode and the one or more sensing electrodes includes at least one mini-electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes at least one mini-electrode and one or more sensing electrodes includes an ablation electrode and a ring electrode.

Additionally or alternatively to any of the examples above, one or more current-carrying electrodes includes an ablation electrode and a mini-electrode and one or more sensing electrodes includes a ring electrode and a mini-electrode.

Additionally or alternatively to any of the examples above, one or more current-injecting electrodes includes a ring electrode and a mini-electrode and one or more sensing electrodes includes an ablation electrode and a mini-electrode.

Another example electrophysiology medical device may include a catheter shaft including a distal end portion. The distal end portion includes a plurality of electrodes. The plurality of electrodes includes at least one current-carrying electrode, a first sensing electrode and a second sensing electrode. Further, at least one of the electrodes is a minielectrode disposed on another one of the other electrodes. The first sensing electrode is spaced from the current-carrying electrode a first distance. The second sensing electrode is spaced from the current-carrying electrode a second distance and the first distance is different from the second distance.

Additionally or alternatively to any of the examples above, the medical device may include a controller coupled to the plurality of electrodes. The at least one current-carrying electrode and the first and second sensing electrodes are arranged in a four-terminal sensing configuration and the controller is capable of calculating a parameter capable of indicating the proximity of the medical device to tissue.

An example method for diagnosing and/or treating a condition of the heart may include advancing an electrophysiology catheter through a blood vessel to a position adjacent a target site and utilizing the catheter to determine the proximity of the catheter to the target site. The catheter includes a distal end portion and a four-terminal sensing assembly disposed on the distal end portion. The four-

terminal sensing assembly includes one or more current-carrying electrodes and one or more sensing electrodes. One or more current-carrying electrodes and/or the one or more sensing electrodes includes a mini-electrode. The method may also include a controller coupled to the four-terminal sensing assembly.

The above summary of some embodiments is not intended to describe each disclosed embodiment or every implementation of the present disclosure. The Figures, and Detailed Description, which follow, more particularly exemplify these embodiments.

While multiple embodiments are disclosed, still other embodiments of the present invention will become apparent to those skilled in the art from the following detailed description, which shows and describes illustrative embodiments of the invention. Accordingly, the drawings and detailed description are to be regarded as illustrative in nature and not restrictive.

### BRIEF DESCRIPTION OF THE DRAWINGS

The disclosure may be more completely understood in consideration of the following detailed description in connection with the accompanying drawings, in which:

FIG. 1 is a plan view of an example tissue diagnosis and/or ablation system;

FIG. 2 illustrates an example medical device including a distal tip electrode, a ring electrode and mini-electrodes;

FIG. 3 illustrates an example medical device including a <sup>30</sup> distal tip electrode, a ring electrode and a mini-electrode positioned away from the distal tip electrode and/or ring electrode;

FIG. 4 illustrates an example medical device including a distal tip electrode, a ring electrode and mini-electrodes <sup>35</sup> arranged in a four-terminal sensing configuration;

FIG. 5 illustrates two example medical devices arranged in a four-terminal sensing configuration having one mini-electrode positioned separate from an ablation electrode and/or ring electrode;

FIG. 6 illustrates an example medical device including a distal tip electrode, a ring electrode and mini-electrodes arranged in a three-terminal sensing configuration;

FIG. 7 illustrates an example medical device including a current injecting electrode and four potential measuring 45 electrodes;

FIGS. 8a-8c illustrates an example medical device positioned relative to two different mediums.

While the disclosure is amenable to various modifications and alternative forms, specifics thereof have been shown by 50 way of example in the drawings and will be described in detail. It should be understood, however, that the intention is not to limit the invention to the particular embodiments described. On the contrary, the intention is to cover all modifications, equivalents, and alternatives falling within 55 the spirit and scope of the disclosure.

## DETAILED DESCRIPTION

For the following defined terms, these definitions shall be applied, unless a different definition is given in the claims or elsewhere in this specification.

All numeric values are herein assumed to be modified by the term "about", whether or not explicitly indicated. The term "about" generally refers to a range of numbers that one 65 of skill in the art would consider equivalent to the recited value (e.g., having the same function or result). In many

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instances, the terms "about" may include numbers that are rounded to the nearest significant figure.

The recitation of numerical ranges by endpoints includes all numbers within that range (e.g. 1 to 5 includes 1, 1.5, 2, 2.75, 3, 3.80, 4, and 5).

As used in this specification and the appended claims, the singular forms "a", "an", and "the" include plural referents unless the content clearly dictates otherwise. As used in this specification and the appended claims, the term "or" is generally employed in its sense including "and/or" unless the content clearly dictates otherwise.

It is noted that references in the specification to "an embodiment", "some embodiments", "other embodiments", etc., indicate that the embodiment described may include one or more particular features, structures, and/or characteristics. However, such recitations do not necessarily mean that all embodiments include the particular features, structures, and/or characteristics. Additionally, when particular features, structures, and/or characteristics are described in connection with one embodiment, it should be understood that such features, structures, and/or characteristics may also be used connection with other embodiments whether or not explicitly described unless clearly stated to the contrary.

The following detailed description should be read with reference to the drawings in which similar elements in different drawings are numbered the same. The drawings, which are not necessarily to scale, depict illustrative embodiments and are not intended to limit the scope of the invention.

Cardiac arrhythmia and/or other cardiac pathology contributing to abnormal heart function may originate in cardiac cellular tissue. One technique that may be utilized to treat the arrhythmia and/or cardiac pathology may include ablation of tissue substrates contributing to the arrhythmia and/or cardiac pathology. The tissue in the substrate may be electrically disrupted, or ablated, by heat, chemicals or other means of creating a lesion in the tissue, or otherwise can be electrically isolated from the normal heart circuit. Electrophysiology therapy involves locating the tissue contributing to the arrhythmia and/or cardiac pathology using an ablation, mapping and/or diagnosing catheter and then using the ablation catheter (or another device) to destroy and/or isolate the tissue.

Prior to performing an ablation procedure, a physician and/or clinician may utilize specialized mapping and/or diagnostic catheters to precisely locate tissue contributing and/or causing an arrhythmia or other cardiac pathology. It may, therefore, be desirable to be able to precisely locate the targeted tissue prior to performing the ablation procedure in order to effectively alleviate and/or eliminate the arrhythmia and/or cardiac pathology. Further, precise targeting of the tissue may prevent or reduce the likelihood that healthy tissue (located proximate the targeted tissue) is damaged.

Several methods and/or techniques may be employed to precisely locate targeted tissue where an ablation or other therapeutic procedure may be performed. An example method may include utilizing an ablation, mapping and/or diagnostic catheter to determine how close the catheter is to targeted tissue. Further, the ablation, mapping and/or diagnostic catheter may include one or more sensing electrodes located on a distal portion of the catheter. The electrodes may sense, measure and/or provide a controller with information relating to electrical activity within the cardiac tissue. Using the sensed and/or measured electrical information from cardiac tissue, the controller may be able to correlate the spatial location of the distal portion of the catheter in relation to the cardiac tissue. For example, the

electrodes may measure the impedance, resistance, voltage potential, etc. and determine how far a distal portion of a diagnostic and/or ablation catheter is to cardiac tissue.

Electrodes utilized in conjunction with an ablation, mapping and/or diagnostic catheter are often located on the distal portion and/or distal end of the catheter. For example, an ablation catheter may include a distal tip electrode and one or more ring electrodes located proximal the distal tip electrode. The distal tip electrode may be able to sense and/or measure electrical activity in addition to being able to provide ablative therapy as an ablation electrode. The ring electrodes may be used as sensing and/or measuring electrodes in conjunction with one another and/or the ablation electrode.

In general, the size and/or spacing of electrodes may 15 contribute to the accuracy of the electrical information sensed and/or measured by the mapping and/or diagnostic catheter. For example, some methods and/or techniques may emit a current from a first electrode and measure the impedance (or other electrical characteristic) of local tissue 20 using a different pair of electrodes. However, a current emitted from an electrode having a large surface area may not be as concentrated as compared to a current emitted from an electrode having a (proportionally) smaller surface area. A smaller electrode surface area may have a tendency to 25 focus and/or direct current to tissue immediately adjacent the emitting and/or measuring electrodes.

Further, in some circumstances it may be challenging to position an ablation tip and/or ring electrodes precisely adjacent targeted tissue due to the relatively large size of the 30 tip and/or a ring electrode. In particular, it may be challenging to arrange larger electrodes in an optimally-spaced configuration because the size and shape of larger electrodes may limit how close the electrodes can be placed to one another.

In addition, larger electrodes may be more susceptible (as compared to smaller electrodes) to detecting far field electrical activity. Detection of far field electrical activity may negatively affect the detection of local (e.g. targeted) electrical activity.

Therefore, it may be desirable in some instances to utilize, dispose, incorporate and/or couple smaller electrodes (e.g. mini-electrodes) into the distal portion of mapping and/or diagnostic catheters. For example, some of the medical devices and methods disclosed herein may include sensing 45 and measuring electrical activity using mini-electrodes alone or in conjunction with ablation electrodes, ring electrodes, catheters and/or other medical devices. Further, some of the medical devices and methods disclosed herein may utilize electrical information collected from mini-electrodes 50 to assess tissue proximity and/or contact. Other methods and medical devices are also disclosed.

FIG. 1 illustrates an example cardiac mapping and/or ablation system 10. As shown in FIG. 1, system 10 may include an elongated member or catheter shaft 12, an RF 55 generator 14, and a controller 16 (e.g., a mapping processor, ablation processor, and/or other processor). Illustratively, shaft 12 may be operatively coupled to at least one or more (e.g., one or both) of RF generator 14 and controller 16. Alternatively, or in addition, a device (other than shaft 12), 60 may be utilized to apply ablation energy and/or diagnose a target area and may be operatively coupled to at least one or more of RF generator 14 and controller 16. RF generator 14 may be capable of delivering and/or may be configured to deliver ablation energy to shaft 12 in a controlled manner in 65 order to ablate target area sites identified by controller 16. Although the controller 16 and RF generator 14 may be

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shown as discrete components, these components or features of components may be incorporated into a single device. System 10 may include any of one or more other features, as desired.

In at least some embodiments, shaft 12 may include a handle 18, which may have an actuator 20 (e.g., a control knob or other actuator). The handle 18 (e.g., a proximal handle) may be positioned at a proximal end of shaft 12, for example. Illustratively, shaft 12 may include a flexible body having a having a distal portion which may include one or more electrodes. For example, the distal portion of shaft 12 may include one or more of a plurality of ring electrodes 22, a distal ablation tip electrode 24, and a plurality of minielectrodes 26 disposed or otherwise positioned along and/or electrically isolated from distal ablation tip electrode 24.

Shaft 12 may be steerable to facilitate navigating the vasculature of a patient or navigating other lumens. Illustratively, a distal portion 13 of shaft 12 may be deflected by manipulation of actuator 20 to effect steering shaft 12. In some instances, distal portion 13 of shaft 12 may be deflected to position distal ablation tip electrode **24** and/or mini-electrodes 26 adjacent target tissue or to position the distal portion 13 of shaft 12 for another suitable purpose. Additionally, or alternatively, distal portion 13 of shaft 12 may have a pre-formed shape adapted to facilitate positioning distal ablation tip electrode 24 and/or micro-electrode assemblies 26 adjacent a target tissue. Illustratively, the preformed shape of distal portion 13 of shaft 12 may be a radiused shape (e.g., a generally circular shape or a generally semi-circular shape) and/or may be oriented in a plane transverse to a general longitudinal direction of shaft 12. These are just examples.

In some instances, system 10 may be utilized in ablation procedures on a patient. Illustratively, shaft 12 may be configured to be introduced into or through vasculature of a patient and/or into or through any other lumen or cavity. In one example, shaft 12 may be inserted through the vasculature of the patient and into one or more chambers of the patient's heart (e.g., a target area). When in the patient's vasculature or heart, shaft 12 may be used to map and/or ablate myocardial tissue using the ring electrodes 22, minielectrodes 26, and/or distal ablation tip electrode 24. In some instances, distal ablation tip electrode 24 may be configured to apply ablation energy to myocardial tissue of the heart of a patient.

Distal ablation tip electrode **24** may be a suitable length and include a suitable surface area. In some instances, distal ablation tip electrode **24** may have a length of between one (1) mm and twenty (20) mm, three (3) mm and seventeen (17) mm, or six (6) mm and fourteen (14) mm. In one illustrative example, distal ablation tip electrode **24** may have an axial length of about eight (8) mm. Further, distal ablation tip electrode may have a suitable surface area of between five (5) mm² and one hundred (100) mm², ten (10) mm² and eighty (80) mm², or twenty (20) mm² and seventy (70) mm². In one illustrative example, distal ablation tip electrode **24** may have a surface area of about twenty-nine (29) mm². Distal ablation tip electrode **24** may be formed from or otherwise include platinum and/or other suitable materials. These are just examples.

As stated, mini-electrodes 26 may be circumferentially distributed about a distal ablation tip electrode 24. Mini-electrodes 26 may be capable of operating, or configured to operate, in unipolar or bipolar sensing modes. Mini-electrodes 26 may be capable of sensing, or may be configured to sense, electrical characteristics (e.g. impedance) corresponding to myocardial tissue proximate thereto.

For example, in some instances system 10 may be capable of utilizing impedance measurements to sense contact between the catheter tip (e.g. distal ablation tip electrode 24) and tissue. In general, the impedance of a given medium may be measured by applying a known voltage or current to 5 a given medium and measuring the resulting voltage or current. In other words, impedance measurements of a given medium can be obtained by injecting current between two electrodes and measuring the resulting voltage between the same electrodes through which the current was injected. The 10 ratio of the voltage potential to the applied current provides an indication of the impedance of the medium through which the current traveled.

For example, FIG. 1 illustrates that current may be injected between distal ablation tip electrode **24** and a ring 15 electrode 22. Impedance of the medium (e.g. tissue) adjacent to distal ablation tip electrode 24 and ring electrode 22 may be measured according to the methodology disclosed above. For example, if the distal ablation tip electrode **24** and ring electrode are embedded in cardiac tissue, the impedance of 20 the cardiac tissue may be determined.

In some instances, contact system 10 may utilize different impedance measurements of a local medium to determine whether the distal ablation tip electrode 24 is contacting tissue. For example, the impedance of cardiac tissue is 25 different than that of blood. Therefore, by knowing the relative difference in the impedance of tissue versus blood, system 10 may be able to determine whether the medium through which a current is being applied is either blood or cardiac tissue, for example.

In some examples, mini-electrodes 26 may be operatively coupled to controller 16. Further, generated output from mini-electrodes 26 may be sent to controller 16 of system 10 for processing in one or more manners discussed herein trical characteristic (e.g. impedance) and/or an output signal from a mini-electrode pair may at least partially form the basis of a contact assessment, ablation area assessment (e.g., tissue viability assessment), and/or an ablation progress assessment (e.g., a lesion formation/maturation analysis), as 40 discussed below.

Further, system 10 may be capable of processing or may be configured to process the electrical signals from minielectrodes 26, ring electrodes 22, and/or distal ablation tip electrode **24**. Based, at least in part, on the processed output 45 from mini-electrodes 26, ring electrodes 22, and/or distal ablation tip electrode 24, controller 16 may generate an output to a display (not shown) for use by a physician or other user. In instances where an output is generated to a display and/or other instances, controller 16 may be opera- 50 tively coupled to or otherwise in communication with the display. Illustratively, the display may include various static and/or dynamic information related to the use of system 10. In one example, the display may include one or more of an image of the target area, an image of shaft 12, and/or 55 indicators conveying information corresponding to tissue proximity, which may be analyzed by the user and/or by a processor of system 10 to determine the existence and/or location of arrhythmia substrates within the heart, to determine the location of shaft 12 within the heart, and/or to make 60 other determinations relating to use of shaft 12 and/or other elongated members.

System 10 may include an indicator in communication with controller 16. The indicator may be capable of providing an indication related to a feature of the output signals 65 received from one or more of the electrodes of shaft 12. In one example, an indication to the clinician about a charac-

teristic of shaft 12 and/or the myocardial tissue interacted with and/or being mapped may be provided on the display. In some cases, the indicator may provide a visual and/or audible indication to provide information concerning the characteristic of shaft 12 and/or the myocardial tissue interacted with and/or being mapped. For example, system 10 may determine that a measured impedance corresponds to an impedance value of cardiac tissue and therefore may output a color indicator (e.g. green) to a display. The color indicator may allow a physician to more easily determine whether to apply ablative therapy to a given cardiac location. This is just an example. It is contemplated that a variety of indicators may be utilized by system 10.

In the above disclosure, the ability for system 10 to accurately measure impedance values may depend on the relative distribution of current density being applied to a given medium. For example, the size of the electrode from which current is emitted may lead to current diffusion through non-targeted, surrounding tissue. When comparing the current density of two electrodes, one of which is proportionally larger than the other, the electrode with less surface area may concentrate an electrical current to localized tissue to a greater extent than the larger electrode. Therefore, it may be challenging to get accurate current delivery at discrete spatial points in cardiac tissue when utilizing proportionally larger electrodes.

Additional details regarding mini-electrodes 26, distal ablation tip electrode 24 and ring electrode 22 are shown in FIG. 2. FIG. 2 illustrates that mini-electrodes 26 may include "inner" electrode 28. Further, a layer of insulation 32 may be disposed around inner electrode 28. In embodiments where mini-electrodes 26 are disposed along distal ablation tip electrode 24, insulation 32 may insulate inner electrode 28 from distal ablation tip electrode 24, ring electrode 22 and/or for processing in other manners. As stated, an elec- 35 and/or other inner electrodes 28. In some embodiments, insulation 32 may surround and isolate inner electrode 28 from ablation tip electrode **24**.

> As shown in FIG. 2, mini-electrodes 26 may be positioned such that there is minimal space between adjacent minielectrodes 26. Further, the smaller size of mini-electrodes 26 (relative to distal ablation tip electrode 24, for example) may allow mini-electrodes to be positioned in multiple configurations. For example, mini-electrodes 26 may circumferentially aligned as shown in FIG. 2. Additionally, mini-electrodes 26 may be offset in a variety of different configurations. For example, mini-electrodes 26 may be positioned longitudinally along the longitudinal axis of shaft 12 or may be positioned on the apex of distal ablation tip electrode 24.

> It is contemplated that mini-electrodes 26 may have a suitable exposed surface area of between 0.20 mm<sup>2</sup> and 1 mm<sup>2</sup>, 0.30 mm<sup>2</sup> and 0.80 mm<sup>2</sup>, or 0.40 mm<sup>2</sup> and 0.70 mm<sup>2</sup>. In one embodiment, mini-electrodes 26 may have a suitable exposed surface area of 0.50 mm<sup>2</sup>. Comparison of the ratio of the suitable exposed surface are of mini-electrodes 26 to that of distal ablation tip electrode **24** shows that the suitable exposed surface area of distal ablation tip electrode 24 may be at least ten (10) times larger, fifteen (15) times, or twenty (20) times larger than the suitable surface are of minielectrodes 26. These are just examples. The ratio of the suitable exposed surface area of distal tip electrode 24 to the suitable exposed surface area of mini-electrode 26 may be less than or greater than twenty (20). For example, the ratio of the suitable exposed surface area of distal tip electrode 24 to the suitable exposed surface area of mini-electrode 26 may be 30, 50, or 100. Further, the ratio of the suitable exposed surface area of distal tip electrode 24 to the suitable

exposed surface area of mini-electrode 26 may be less than one hundred seventy five (175).

Alternatively, mini-electrodes 26 may be used in conjunction with distal ablation tip electrode 24, with ring electrode 22, or alone. Additionally, because mini-electrodes 26 may 5 be proportionally smaller than either distal ablation tip electrode 24 and/or ring electrode 22, mini-electrodes 26 may be positioned in many different spatial configurations with respect to distal ablation tip electrode 24 and/or ring electrode 22. For example, as shown in FIG. 2, mini- 10 electrodes 26 may be disposed "on" distal ablation tip electrode 24. As discussed herein, mini-electrodes 26 may be described as being "on," "along," and/or otherwise embedded and/or encased on a given structure. This is not intended to be limiting. Rather, mini-electrodes 26 can be 15 positioned and/or otherwise located at any suitable position/ location along the distal tip and/or at other locations along the catheter and/or other remote structure. Positioning/locating the electrodes may include embedding, partially embedding, encasing, partially encasing, isolating, attach- 20 ing, affixing, fastening, bonding to the outer surface, embedding within the wall, or the like.

Even though much of the discussion herein has been directed to embodiments in which mini-electrodes 26 have been positioned "on" distal ablation tip electrode **24**, it is 25 further contemplated that one or more mini-electrodes may be positioned along the catheter shaft at a position that is away from distal ablation tip electrode 24 and continue to function substantially equivalent to those embodiments in which mini-electrodes are positioned "on" distal tip ablation 30 electrode 24.

For example, FIG. 3 shows mini-electrode 26 disposed on shaft 12 away from distal ablation tip electrode 24. Further, as discussed above, mini-electrode 26 disposed away from catheter shaft 12 or any other portion of ablation system 10. Additionally, mini-electrodes 26 may be "on" other electrodes (e.g. ring electrode, etc.). As stated above, minielectrode 26 may be substantially smaller than distal ablation tip electrode 24. As illustrated in FIG. 3, mini-electrode 40 26 is substantially smaller than distal ablation tip electrode **24**.

Further, the size of mini-electrodes 26 may allow minielectrodes 26 to be placed directly adjacent to tissue for which an ablation, diagnostic and/or therapeutic procedure 45 may be performed. For example, as discussed above, in order to determine tissue contact through impedance measurements, the current for which a voltage ratio (and hence, impedance) is measured must pass through the medium (e.g. tissue) for which the targeted impedance value is sought. If 50 the current is diffused and/or passes primarily through a non-targeted medium (e.g. blood), the observed impedance value may not accurately represent whether the catheter is in contact with the desired medium (e.g. tissue).

Due to their relatively small size, mini-electrodes **26** may 55 be placed precisely at a discrete point in space. Further, it may be desirable to inject current between mini-electrodes 26 positioned at a discrete point in space. It can be appreciated that measurements (e.g. impedance) derived from mini-electrodes 26 may reflect the medium adjacent to a 60 discrete point in space. For example, positioning and driving current through closely positioned mini-electrodes 26 may provide greater confidence that impedance measurements derived therefrom are accurate.

Further, it may be desirable to position mini-electrodes **26** 65 close to distal ablation tip electrode 24 and/or ring electrode 22. For example, disposing closely-positioned mini-elec**10** 

trodes 26 directly on distal ablation tip 24 may provide confidence that distal ablation tip **24** is, in fact, in contact with a given medium reflected by a particular impedance measurement.

As stated above, injecting current through mini-electrodes 26 (versus a larger distal ablation tip electrode 24 and/or ring electrode 22) may improve measurements by concentrating the current path precisely through a localized medium. Diffusion of current through surrounding tissue may be reduced by injecting current through the smaller surface area of mini-electrode 26 verses a larger surface area electrode.

Additionally or alternatively, improvement in the measurement of impedance may be accomplished by using a four-terminal sensing configuration. In general, a four-terminal sensing configuration drives current through a pair of electrodes (similar to that discussed above) and measures the voltage across a different pair of electrodes. For ease of understanding the foregoing discussion, the electrode pair between which current is injected in a four-terminal sensing configuration will be hereafter referred to as the "currentcarrying" electrode pair. The electrode pair across which voltage is measured will be referred to as the "sensing" electrode pair.

One advantage of a four-terminal sensing configuration is that the measured impedance may not be sensitive to the impedance of the electrodes. In a two-terminal sensing configuration, the measured impedance includes the surrounding medium and both electrodes. In contrast, a fourterminal sensing configuration measures voltage across electrodes through which the current is negligible. As a result, the measured impedance is that of the surrounding medium and is largely independent of the impedance of the electrode and its interface with the surrounding medium.

For example, FIG. 4 illustrates a four-terminal sensing distal ablation tip electrode 24 may be positioned "on" 35 configuration using distal ablation tip electrode 124, ring electrode 122 and two mini-electrodes 126. Additionally, FIG. 4 shows lead wires 132*a*-132*d*. Lead wires 132*a*-132*d* may connect any given electrode to controller 16, RF generator 14 or both. Lead wires 132a-132d may also connect individual electrodes to one another in a variety of configurations.

Referring to FIG. 4, the distal ablation tip electrode 124 and ring electrode 122 may define the current-carrying electrode pair. Further, the pair of mini-electrodes 126 may define the sensing electrode pair. Therefore, current may be injected between the distal ablation tip electrode 126 and the ring electrode 122, and voltage may be measured across mini-electrodes 126. It can be appreciated that in this example, impedance measurements may be the impedance of the medium adjacent the sensing electrode pair. For example, if the distal portion 13 of system 10 is embedded in tissue, mini-electrodes 126 may measure the impedance of tissue adjacent mini-electrodes 126. It should be understood that one advantage of using a four-terminal system with mini-electrodes 126 is that precise measurements of impedance (or other electrical characteristics) may be obtained at a discrete point.

Additionally or alternatively, a variety of combinations, arrangements and/or configurations may incorporate a variety of electrodes (e.g. distal ablation tip electrode, ring electrode, mini-electrode, remote reference electrode, etc.) in a four-terminal sensing configuration. In some combinations (e.g. the combinations illustrated in FIG. 3 or FIG. 4), the electrodes may be disposed on distal portion 13/113 of catheter shaft 12/112. In other combinations, one or more of the electrodes in a four-terminal sensing configuration may not be disposed on catheter shaft 12/112 and/or distal portion

13/113. Rather, some electrodes may be located off of and away from catheter shaft 12/112 and/or distal portion **13/113**.

For example, FIG. 5 shows electrode 134 located away from catheter shaft 112 and distal portion 113. In this 5 example, electrode 134 is located on catheter shaft 136, which is different from or otherwise separate from catheter shaft 112. Even though FIG. 5 shows electrode 134 disposed on catheter shaft 136, it is contemplated that electrode 134 may be located or disposed on any structure away from 10 catheter shaft 112. For example, electrode 134 may be disposed on the surface of a patient's body or disposed on another portion of ablation system 10. These are just examples, other combinations and/or remote structures are contemplated.

Similar to that discussed above with respect to FIGS. 2-4, one or more of the electrodes in a four-terminal sensing configuration that are remote and/or disposed away from catheter shaft 112 may be positioned "on" the structure in electrode may be disposed on another electrode yet operate independently of the electrode on which it is disposed (e.g. mini-electrodes 126 disposed on and insulated from distal ablation tip electrode 124).

Additionally or alternatively, a four-terminal sensing con- 25 figuration may be implemented and/or configured using only three electrodes. In some instances, a single electrode (e.g. distal ablation tip electrode, ring electrode, mini-electrode, remote electrode, etc.) may operate as both a currentcarrying and sensing electrode. In this case, the measured 30 impedance may include the impedance of the electrode used for both purposes (e.g., current-carrying and sensing) as well as the impedance of the electrode's interface with the surrounding medium. This configuration may approximate electrode is low or is not expected to vary significantly. Including the impedance of one of the electrodes (and its interface) may be desirable in some cases, particularly if that impedance varies significantly with tissue contact.

FIG. 6 illustrates a three-terminal sensing configuration. In FIG. 6, any one of distal ablation tip electrode 124, mini-electrode 126 or ring electrode 122 may operate as both a current-carrying and sensing electrode. Further, any of the embodiments and/or configurations discussed with respect to FIGS. 2-5 (e.g. the four-terminal sensing configuration) may be implemented in the three-terminal configuration.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include one or more mini-electrodes 126, while the sensing electrode pair 50 may include the distal tip ablation electrode 124 and/or ring electrode 122.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include a distal tip ablation electrode 124 and a mini-electrode 126, while the sensing electrode pair may include one or more minielectrodes 126.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include one or more mini-electrodes 126, while the sensing electrode pair 60 may include a distal tip ablation electrode 124 and one or more mini-electrodes 126.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include one or more mini-electrodes 126, while the sensing electrode pair 65 may include a ring electrode 122 and one or more minielectrodes 126.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include a ring electrode 122 and one or more mini-electrodes 126, while the sensing electrode pair may include one or more minielectrodes 126.

In another example of a four-terminal sensing configuration, all the electrodes in the four-terminal sensing configuration may be mini-electrodes 126.

In another example of a four-terminal sensing configuration, the current-carrying electrode pair may include one mini-electrode 126 and distal tip ablation electrode 124, while the sensing electrode pair may include one or more mini-electrode 126 and ring electrode 122.

In another example of a four-terminal sensing configura-15 tion, the sensing electrode pair may include one minielectrode 126 and distal tip ablation electrode 124, while the current-carrying electrode pair may include one or more mini-electrode 126 and ring electrode 122.

In another example of a four-terminal sensing configurawhich they are disposed. Further, as stated above, any given 20 tion, the current-carrying electrode pair may include one mini-electrode 126, while the sensing electrode pair may include the distal tip ablation electrode 124.

> In another example of a four-terminal sensing configuration, the sensing electrode pair may include one minielectrode 126, while the current-carrying electrode pair may include the distal tip ablation electrode 124.

> It is contemplated that the controller 16 may incorporate an algorithm that controls the various electrodes in the desired manner in order to assess contact. This might include powering the electrodes in the manner disclosed herein. This may also include more than one sensing configuration, with the sensing configurations multiplexed in time, frequency, or both.

While the above discussion indicates that mini-electrodes the four-terminal configuration if the impedance of the 35 may be used for tissue contact sensing, this is not intended to be limiting. Rather, the mini-electrodes may be used for a variety of functions including ablation, mapping, sensing, or the like.

> As stated, the impedance, resistance, voltage and/or other output obtained from any of the above described fourterminal sensing configurations may be displayed for diagnostic use by a physician or clinician. For example, a four-terminal sensing configuration may measure and/or sense the impedance of tissue, and output a corresponding indicator (as described above) to a display. The display may be connected to controller 16, RF generator 14 and/or to any other component of system 10.

> In addition or alternatively to that disclosed above, another method for assessing tissue contact may include determining a parameter of a model and observing changes in the parameter as the distal end portion 13 of catheter 12 moves between different mediums (e.g. as between blood and tissue).

> For example, a scaling factor may be a parameter in a model used for this purpose. The model may relate to one or more potential differences between one or more sensing electrodes and a reference electrode. A reference electrode may be an electrode placed a distance away from the potential measuring electrodes. For example, a reference electrode may be placed on the back of a patient.

> Sensing electrodes may be disposed on the tip and/or end of distal portion 13 of a catheter. In some examples, sensing electrodes may include mini-electrodes as described herein.

> Additionally or alternatively, the model may also relate to the distance in space between a current-carrying electrode and one or more sensing electrodes. The current-carrying electrode may take a variety of forms. For example, the

current-carrying electrode may be a distal ablation tip electrode **24** as shown in FIG. **1**. Additionally or alternatively, the current-carrying electrode may include mini-electrodes and/or ring electrodes as described above with reference to FIGS. **1** and **2**.

In some configurations, the potential measurement between a sensing electrode and a reference electrode may be modeled as being inversely proportional to the distance between a current-carrying electrode and a sensing electrode. For example, the relationship may be modeled as:

$$\varphi_{SEi} = \frac{K}{\|r_{CCE1} - r_{SEi}\|} + C$$

In this example, the parameter K may be used to assess tissue contact. The above equation is just an example. Other models and parameters are contemplated.

As stated above, the model may relate to both the potential differences between one or more sensing electrodes and the distance between a current-carrying electrode and sensing electrodes. For example, FIG. 4 illustrates an example distal end portion 213 including a current-carrying electrode 224 and four sensing electrodes 226, 234, 236 and 222. FIG. 4 also shows lead wires 232a-232e. It can be appreciated that the sensing electrodes 226, 234 and 236 may include mini-electrodes while the current-carrying electrode 224 may include a distal ablation tip electrode. Sensing electrodes 226, 234 and 236 may be disposed on distal tip 30 ablation electrode 224. Further, a fourth sensing electrode 222 may be positioned proximate electrodes 224, 226, 234 and 236. Referring to FIG. 4, potential measuring electrode 222 may be a ring electrode. FIG. 4 is just an example. Combinations and configurations of a variety of electrode types may be utilized as either the sensing and/or currentcarrying electrodes.

In some instances, the relationship between the above electrodes and potential values may be represented by the following equation:

$$\begin{bmatrix} \varphi_{SE1} \\ \varphi_{SE2} \\ \varphi_{SE3} \\ \varphi_{SE4} \end{bmatrix} = \begin{bmatrix} \frac{1}{||r_{CCE1} - r_{SE1}||} & 1 \\ \frac{1}{||r_{CCE1} - r_{SE2}||} & 1 \\ \frac{1}{||r_{CCE1} - r_{SE3}||} & 1 \\ \frac{1}{||r_{CCE1} - r_{SE4}||} & 1 \end{bmatrix} [K \ C]$$

It can be appreciated that the variables

$$egin{bmatrix} arphi_{SE1} \ arphi_{SE2} \ arphi_{SE3} \ arphi_{SE4} \ \end{bmatrix}$$

represent the measured potential difference between the four sensing electrodes and a reference electrode. Additionally, the potential differences may be determined by system 10. Further, it can be appreciated that  $\|\mathbf{r}_{CCE1} - \mathbf{r}_{SE1}\|$ ,  $\|\mathbf{r}_{CCE1} - \mathbf{r}_{SE3}\|$  and  $\|\mathbf{r}_{CCE1} - \mathbf{r}_{SE4}\|$  represent the absolute 65 value of the distance (in space) between the current-carrying electrode and the four sensing electrodes, respectively. It is

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further understood that these distances may be determined as the position (and distance) for every sensing electrode in relation to the current-carrying electrode is known.

The parameters K and C in the above system of linear equations can be estimated using a number of well-known techniques for optimization or linear regression. For example, least squares can be used to estimate K and C. Other methods are contemplated.

Scaling factor K may be inversely proportional to the conductivity of a given medium. In other words, the scaling factor K will be different for two mediums having different conductivities. For example, the conductivity of blood is greater than that of cardiac tissue, and therefore, the scaling factor K will be lower for blood as compared to cardiac tissue.

Knowing the potential differences and absolute distance values, it may be possible to solve the linear equation set (above) for the scaling factor, K. Is should be noted that in order to solve the disclosed linear equation set, sensing electrodes must be located at different distances away from the current injecting electrode. If, for example, the distances were all identical, then the matrix on the right-hand side of the equation would be singular and result in an infinite number of equally valid solutions. Referring to FIG. 4, it can be seen that sensing electrodes 226, 234, 236 and 222 are located at different distances from current injecting electrode 224.

FIG. 4 illustrates the sensing electrodes 226, 234, 236 and 222 positioned longitudinally along the catheter shaft 12.

However, it is contemplated that the sensing electrodes 226, 234, 236 and 222 may be positioned in a configuration other than along the longitudinal axis and yet still maintain variable distances between the sensing electrodes and the current-carrying electrode. Additionally, in some instances it may be possible to reduce the number of sensing electrodes to two or three and solve the corresponding linear equation set for scaling factor K. In other instances, it may be desirable to increase the number of sensing electrodes; the parameter K can still be estimated using well-known techniques such as least squares.

It can be appreciated from the above discussion that it may be possible to utilize known variables to solve the disclosed linear equation for the scaling factor K. Therefore, system 10 may determine and compare different scaling factor values as the distal end portion 13 of catheter 12 is moved between different mediums (e.g. blood, tissue).

FIGS. 8a-8c illustrates distal end portion 213 positioned within a variety of mediums. For example, FIG. 8a shows distal end portion 213 surround entirely by blood. FIG. 8ab shows distal end portion 213 positioned at a blood/tissue interface. FIG. 8c shows distal end portion 213 partially embedded within tissue. As stated, the generated scaling factor K corresponding to FIGS. 8a-8c may be different for each different medium. The difference in the scaling factors may be utilized as a diagnostic indicator of the proximity of distal end portion 213 to tissue.

The following documents are herein incorporated by reference: U.S. Patent Application Pub. US2008/0243214, U.S. Patent Application Pub. US2014/0058375, U.S. Patent Application Pub. US2013/0190747, U.S. Patent Application Pub. US2013/0060245, and U.S. Patent Application Pub. US2009/0171345.

Various modifications and additions can be made to the exemplary embodiments discussed without departing from the scope of the present invention. For example, while the embodiments described above refer to particular features, the scope of this invention also includes embodiments

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having different combinations of features and embodiments that do not include all of the described features. Accordingly, the scope of the present invention is intended to embrace all such alternatives, modifications, and variations as fall within the scope of the claims, together with all equivalents thereof. 5

We claim:

- 1. An electrophysiology medical device, comprising: a catheter shaft including a distal end portion;
- a sensing assembly located on the distal end portion, the sensing assembly having three or more terminals;
- wherein the sensing assembly includes one or more current-carrying electrodes and more than one sensing electrodes, wherein a first sensing electrode of the more than one sensing electrodes is spaced apart from the one or more current-carrying electrodes by a first 15 distance, wherein a second sensing electrode of the more than one sensing electrodes is spaced apart from the one or more current-carrying electrodes by a second distance, wherein the first distance is different than the second distance;
- wherein at least one of the one or more current-carrying electrodes and the one or more sensing electrodes includes one or more mini-electrodes and one or more non-mini electrodes;
- disposed on at least one of the one or more non-mini electrodes; and
- a controller coupled to the sensing assembly, the controller configured to
  - sensing electrode and a second potential measurement for the second sensing electrode, the first potential measurement being inversely proportional to the first distance and the second potential measurement being inversely proportional to the second 35 distance,
  - determine a scaling factor based on the first distance, the second distance, the first potential measurement, and the second potential measurement, and determine the conductivity of a medium contacting the 40 mini-electrodes. sensing assembly based on the scaling factor.
- 2. The medical device of claim 1, wherein the three or more terminals includes four terminals.
- 3. The medical device of claim 1, wherein one or more of the three or more terminals are disposed along the distal end 45 portion of the catheter shaft.
- **4**. The medical device of claim **1**, wherein one or more of the three or more terminals are disposed along a device separate from the catheter shaft.
- 5. The medical device of claim 1, wherein the one or more 50 current-carrying electrodes includes at least one mini-electrode of the one or more mini-electrodes.
- **6**. The medical device of claim **1**, wherein the one or more sensing electrodes includes one mini-electrode of the one or more mini-electrodes.
- 7. The medical device of claim 1, wherein the one or more current-carrying electrodes includes a mini-electrode of the one or more mini-electrodes and the one or more sensing electrodes includes two mini-electrodes of the one or more mini-electrodes.
- 8. The medical device of claim 1, wherein the one or more current-carrying electrodes includes two mini-electrodes of the one or more mini-electrodes and the one or more sensing electrodes includes a mini-electrode of the one or more mini-electrodes.
- **9**. The medical device of claim **1**, wherein the one or more current-carrying electrodes includes two mini-electrodes of

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the one or more mini-electrodes and the one or more sensing electrodes includes two mini-electrodes of the one or more mini-electrodes.

- 10. The medical device of claim 1, wherein the one or more current-carrying electrodes or the one or more sensing electrodes includes an ablation electrode.
- 11. The medical device of claim 1, wherein the one or more current-carrying electrodes includes an ablation electrode and wherein the one or more sensing electrodes includes an electrode disposed on the ablation electrode.
- 12. The medical device of claim 1, wherein the one or more sensing electrodes includes an ablation electrode and wherein the one or more current-carrying electrodes includes an electrode disposed on the ablation electrode.
- 13. The medical device of claim 1, wherein the one or more current-carrying electrodes or the one or more sensing electrodes includes a ring electrode.
- **14**. The medical device of claim **1**, wherein the one or 20 more current-carrying electrodes includes an ablation electrode and a ring electrode, and wherein the one or more sensing electrodes includes at least one mini-electrode of the one or more mini-electrodes.
- 15. The medical device of claim 1, wherein the one or wherein at least one of the one or more mini-electrodes is 25 more current-carrying electrodes includes at least one minielectrode of the one or more mini-electrodes, and wherein the one or more sensing electrodes includes an ablation electrode and a ring electrode.
  - 16. The medical device of claim 1, wherein the one or determine a first potential measurement for the first 30 more current-carrying electrodes includes an ablation electrode and a mini-electrode of the one or more mini-electrodes and wherein the one or more sensing electrodes includes a ring electrode and a mini-electrode of the one or more mini-electrodes.
    - 17. The medical device of claim 1, wherein the one or more current-injecting electrodes includes a ring electrode and a mini-electrode of the one or more mini-electrodes and wherein the one or more sensing electrodes includes an ablation electrode and a mini-electrode of the one or more
      - 18. An electrophysiology medical device, comprising: a catheter shaft including a distal end portion, wherein the distal end portion includes a plurality of electrodes;
      - wherein the plurality of electrodes includes at least one current-carrying electrode, a first sensing electrode and a second sensing electrode;
      - wherein at least one of the plurality of electrodes is a mini-electrode and at least one of the plurality of electrodes is a non-mini electrode, wherein one or more of the at least one mini-electrode is disposed on one or more of the at least one non-mini electrode;
      - wherein the first sensing electrode is spaced from the at least one current-carrying electrode by a first distance;
      - wherein the second sensing electrode is spaced from the at least one current-carrying electrode by a second distance;
      - wherein the first distance is different from the second distance; and
      - a controller coupled to the plurality of electrodes, the controller configured to:
        - determine a first potential measurement for the first sensing electrode and a second potential measurement for the second sensing electrode, the first potential measurement being inversely proportional to the first distance and the second potential measurement being inversely proportional to the second distance,

determine a scaling factor based on the first distance, the second distance, the first potential measurement, and the second potential measurement, and determine the conductivity of a medium contacting the sensing assembly based on the scaling factor.

19. The medical device of claim 18, further comprising: wherein the at least one current-carrying electrode and the first and second sensing electrodes are arranged in at least one four-terminal sensing configuration.

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